

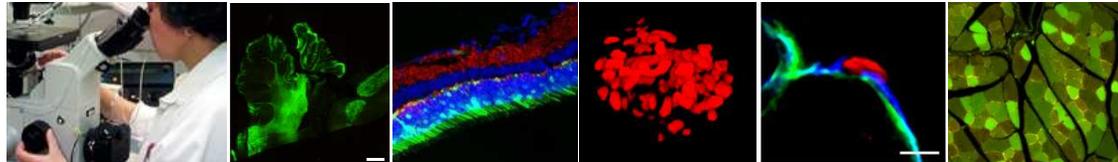
Séminaire SFR santé
11 Décembre, 2012 -

Les nouvelles approches en microscopie pour l'exploration cellulaire et tissulaire

Laurence Dubreil, Plateforme APEX UMR 703 INRA ONIRIS

Philippe Hulin, Plateforme MicroPicell

Steven Nedelec Plateforme MicroPicell



Microscopy of fluorescence

Wide-field

Confocal microscopy

Spectral confocal microscopy

Biphotonic microscopy

TIRF

SIM

STED

PALM and STORM

High Sensitivity and contrast

Multilabelling

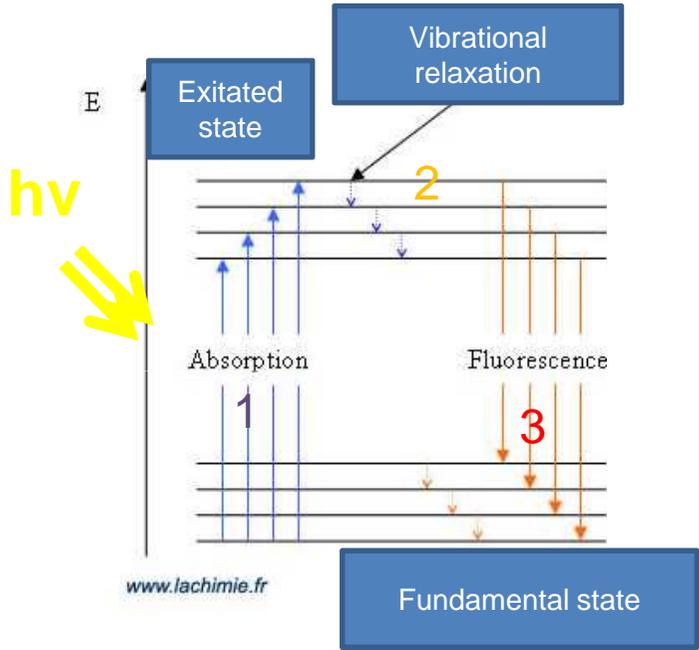
Molecular interactions

Thick specimens and exploration *in vivo*

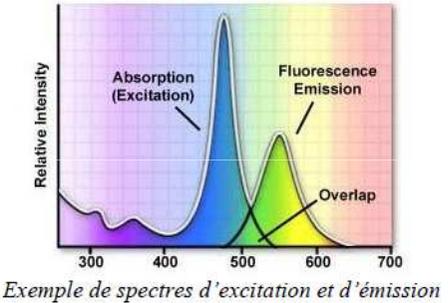
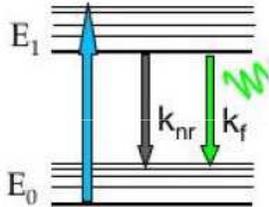
High resolution

Fluorescence : emission of photons

Jablonsky Diagramme

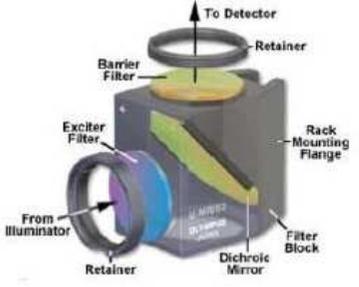


Loi de Stokes
 $E = hc/\lambda$

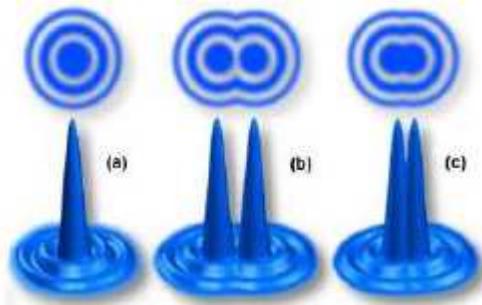


Exemple de spectres d'excitation et d'émission

- 1- stable state to excited state following the absorption of light energy
- 2- vibrational relaxation
- 3- come back to fundamental state S₀ with light energy emission



Resolution limit of an optical system in wide-field



Rayleigh criterion

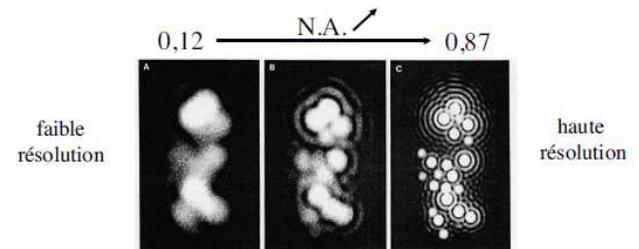
$$R_{xy} = 0,6\lambda/NA$$

$$R_z = 2\lambda/NA^2$$

NA : Numerical Aperture : 1,4
 λ : 488 nm

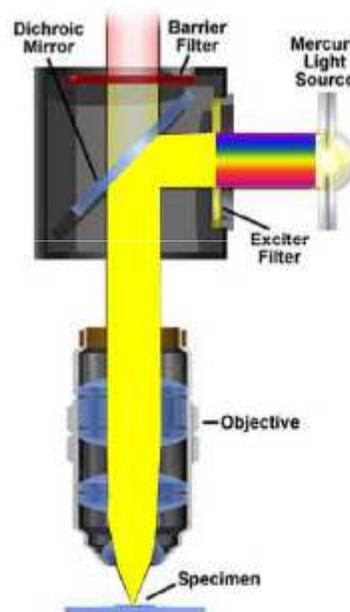
$$d_{xy} = 212,62 \text{ nm}$$

$$d_z = 498 \text{ nm}$$

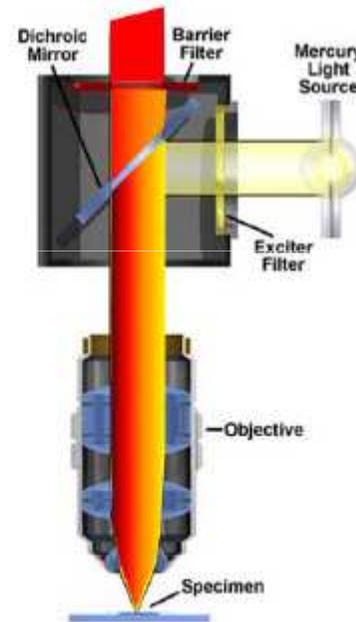


Wide-field fluorescence microscopy

Excitation



Emission

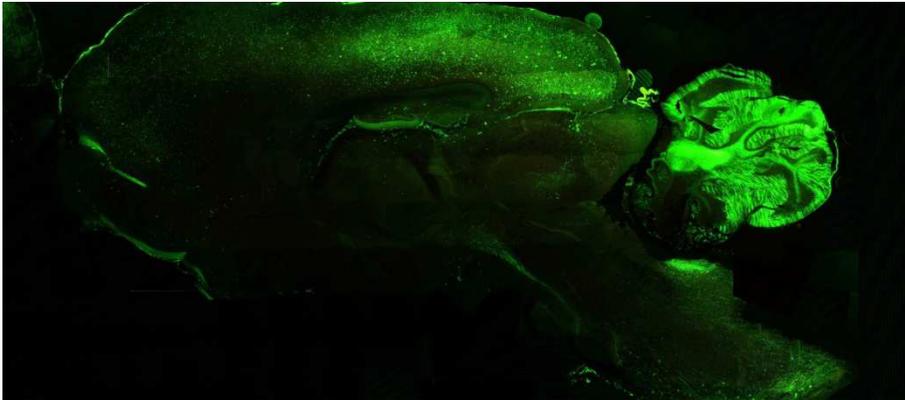


Applications of the wide-field fluorescent microscopy

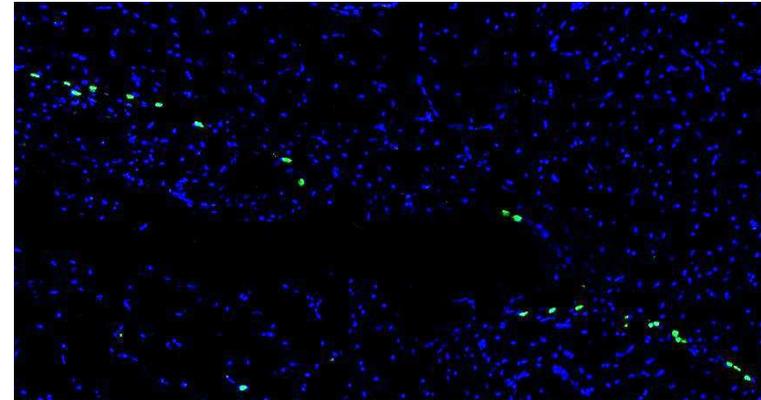
Major input : Large scale analysis, tissular and cellular analysis

Tissular investigation

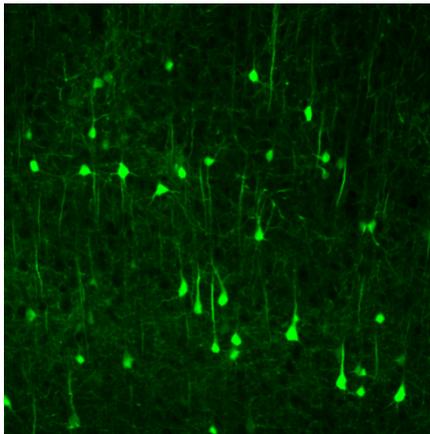
Gene therapy, brain



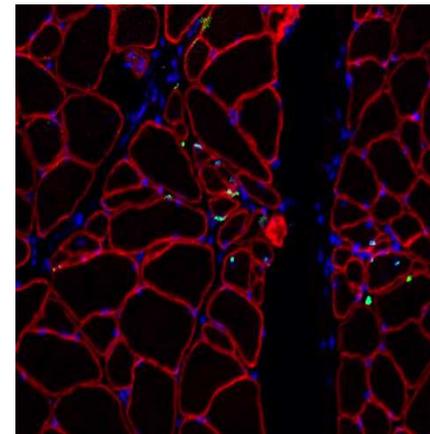
Cell therapy, muscle



Cellular investigation



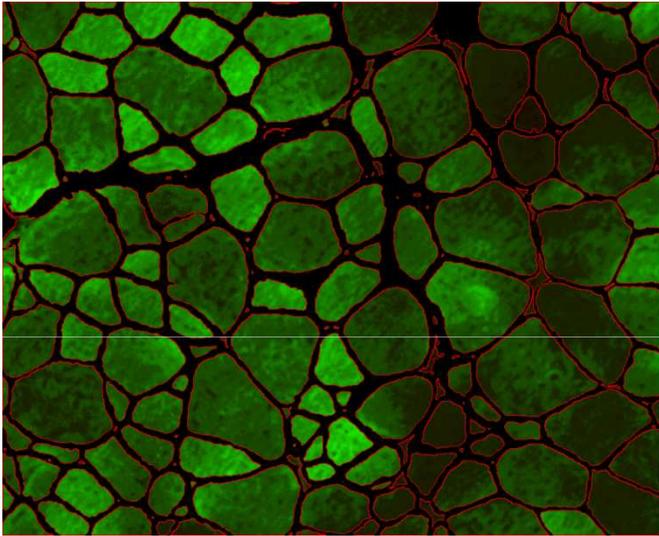
Human lamin A/C immunolabeling on muscle sections



Lamin A/C (green), dystrophin (red)

Applications of the wide-field fluorescent microscopy

Quantification of fluorescence



- Number of transduced fibers
- Fluorescence Intensity

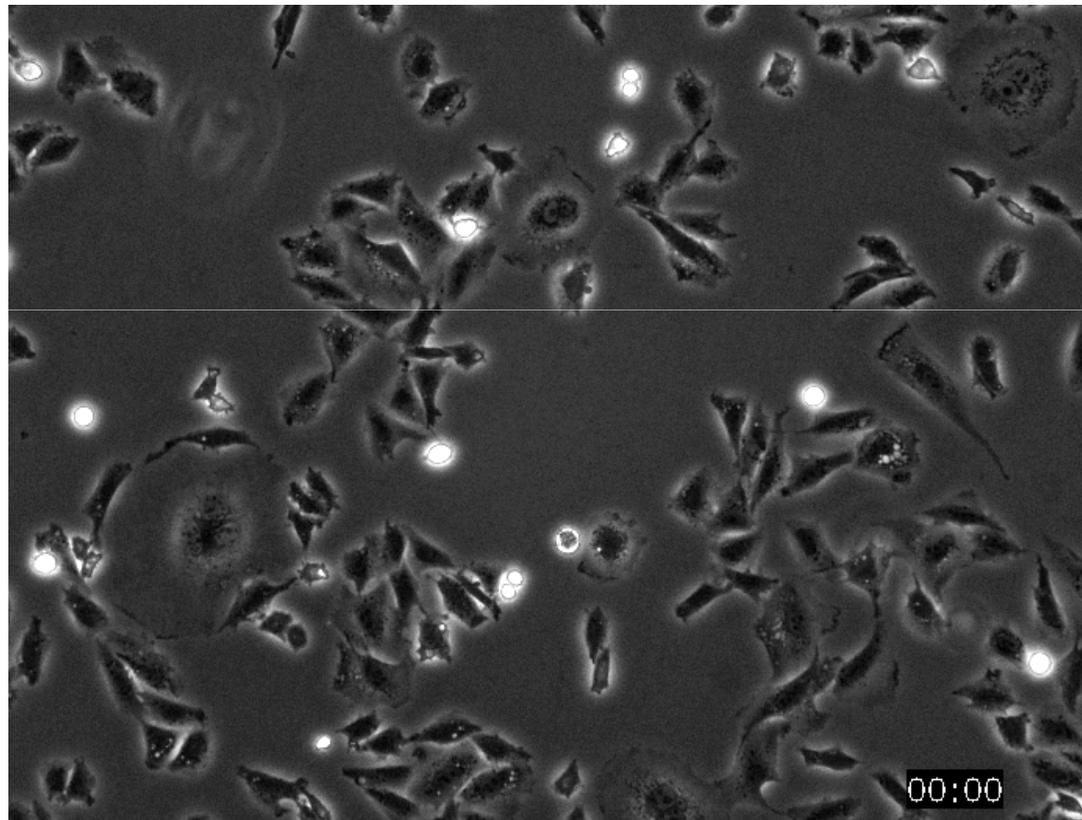
Cryosections of muscle injected with
AAV2/8 RSV-eGFP

Difficulties : Heterogeneity of the GFP fluorescence intensity,
saturation of signal, same threshold for all the specimens,
quality of the sections.

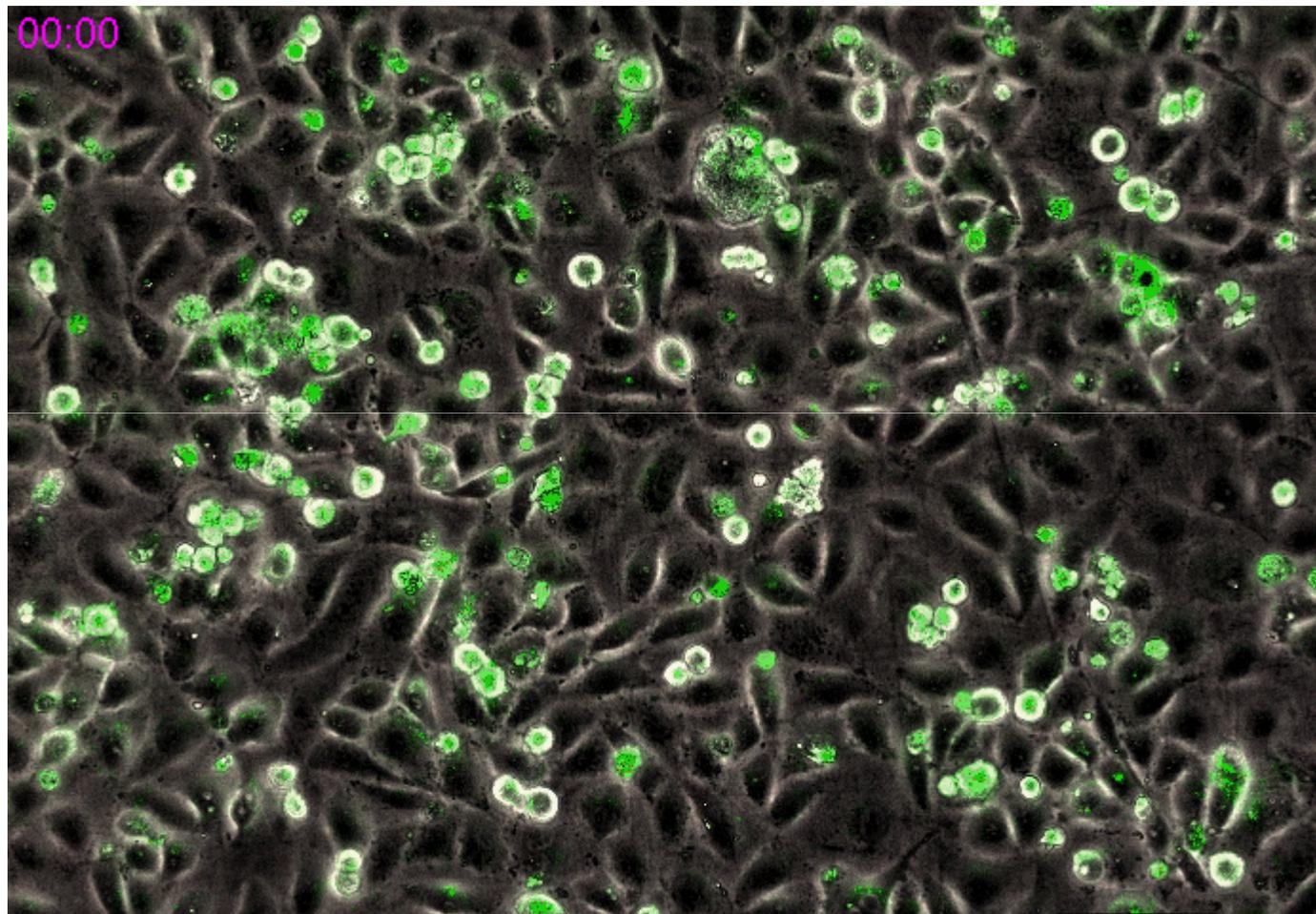
Applications of the wide-field fluorescent microscopy

Cellular « ethology » by video microscopy

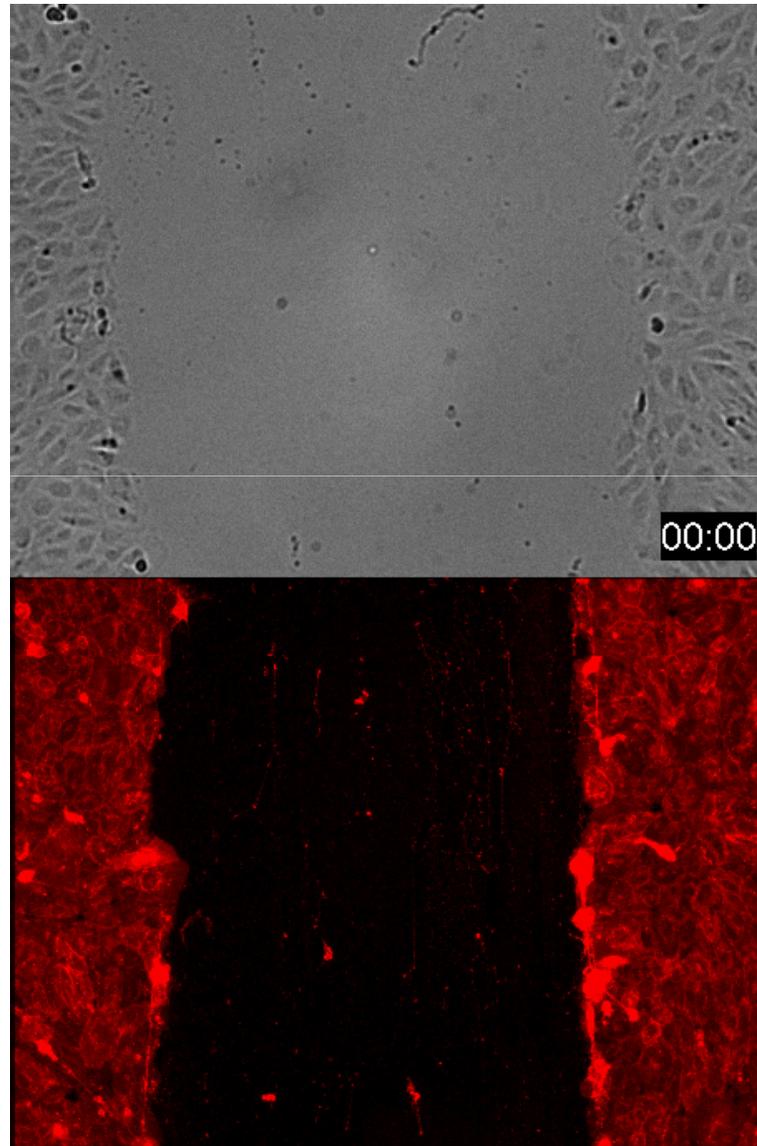
-Time lapse



Applications of the wide-field fluorescent microscopy

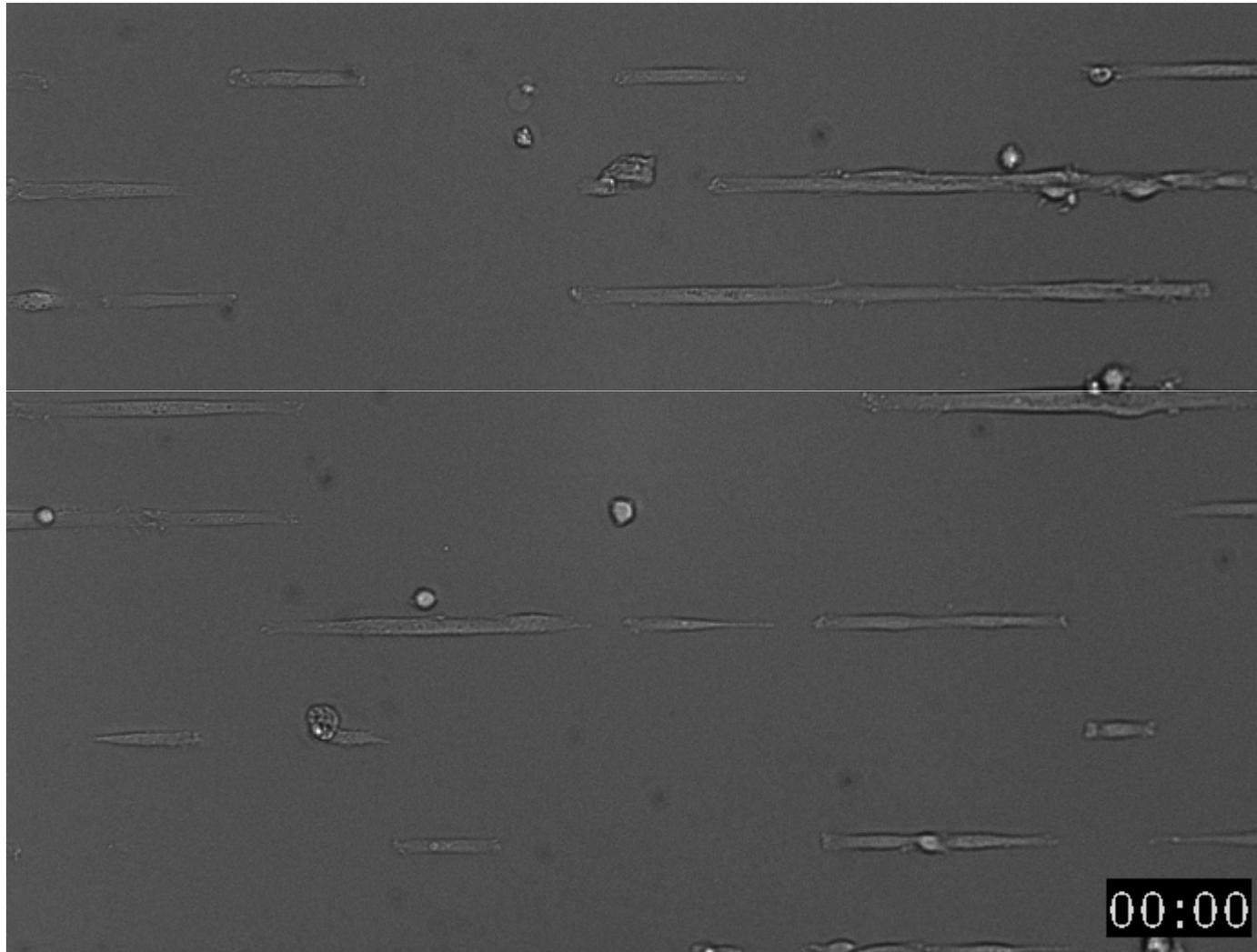


Applications of the wide-field fluorescent microscopy



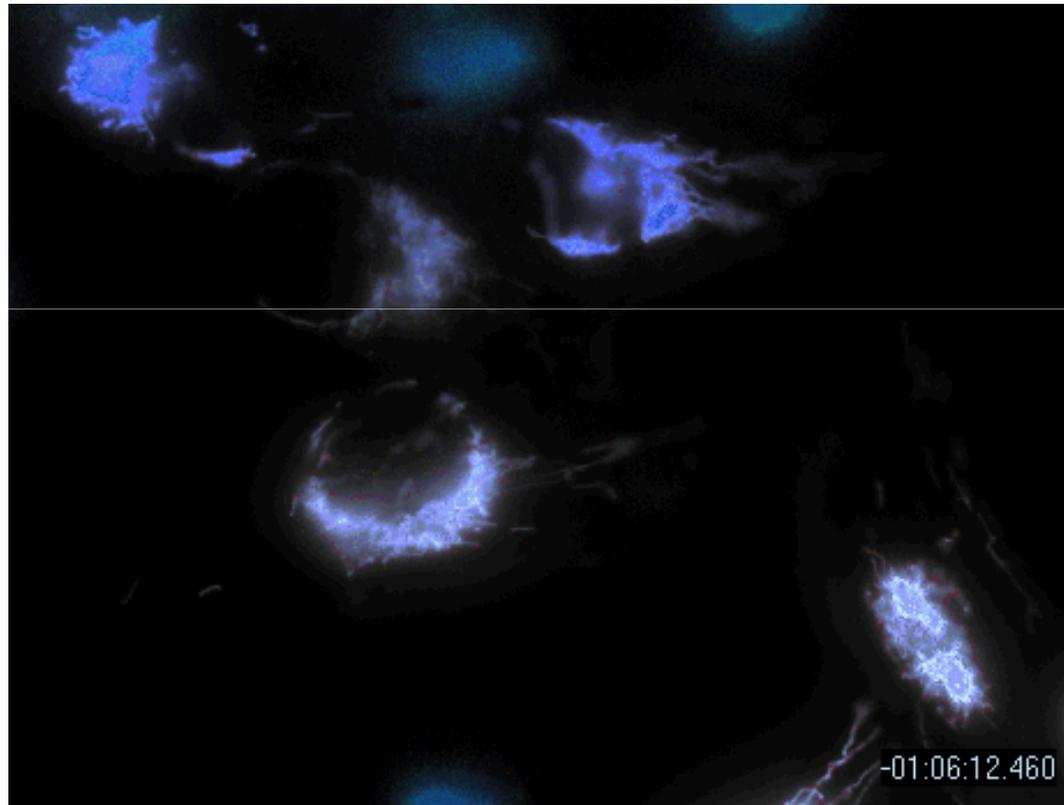
Applications of the wide-field fluorescent microscopy

-Cytosol motility



Applications of the wide-field fluorescent microscopy

-Calcium



Wide-field fluorescence microscopy



High sensitivity

Mercury Light source less energetic than Laser (less photobleaching)

Less expensive than confocal

Multilabeling

Fast acquisition

Video microscopy



Fluorescent emission from all the specimen and not from the focal plane

Limited by the thickness of the specimen

Resolution = $0,6\lambda/NA$

Confocal microscopy

Major input : Increasing of the resolution and monochromatic excitation

$$R_{xy} = 0,4\lambda/NA$$

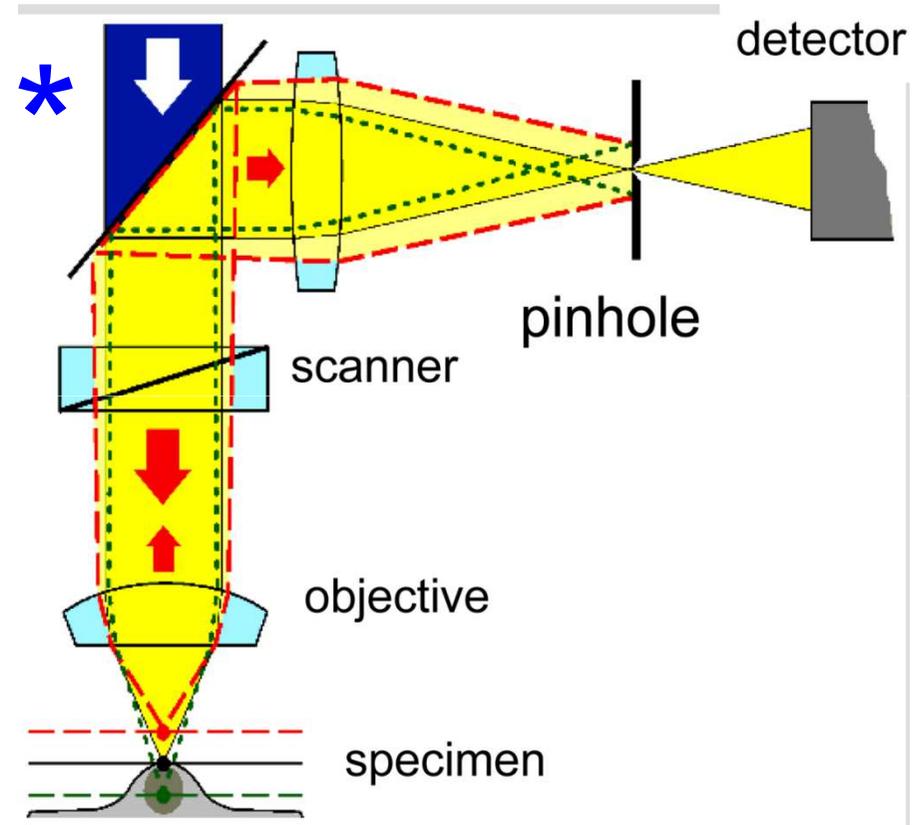
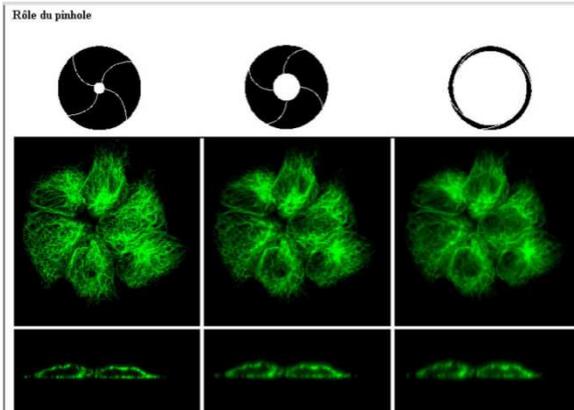
$$R_z = 1,4\lambda/NA^2$$

NA : Numerical Aperture : 1,4

λ : 488 nm

$d_{xy} = 140$ nm

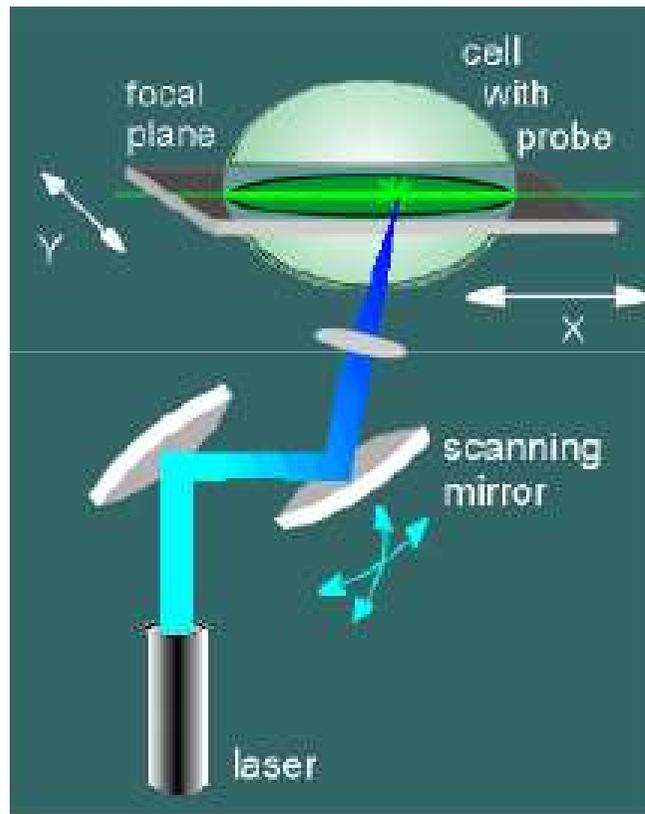
$d_z = 348$ nm



* Monochromatic excitation : Lasers (HeNe), (Arg) ou Diodes

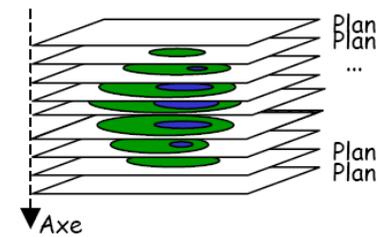
Scanning mirrors

Major input : rate of scanning and 3D imaging



Resonant scanning

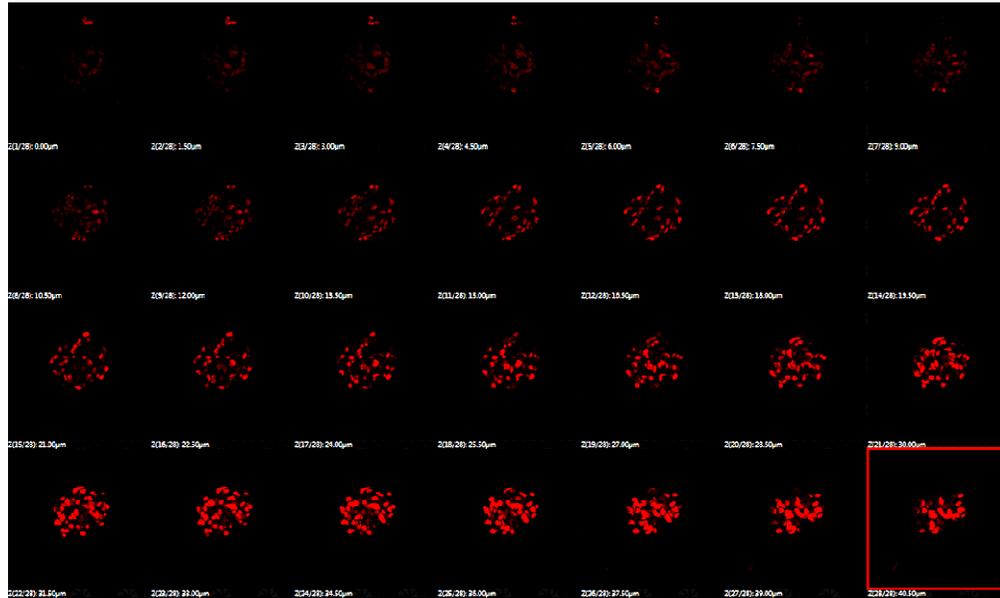
3D building



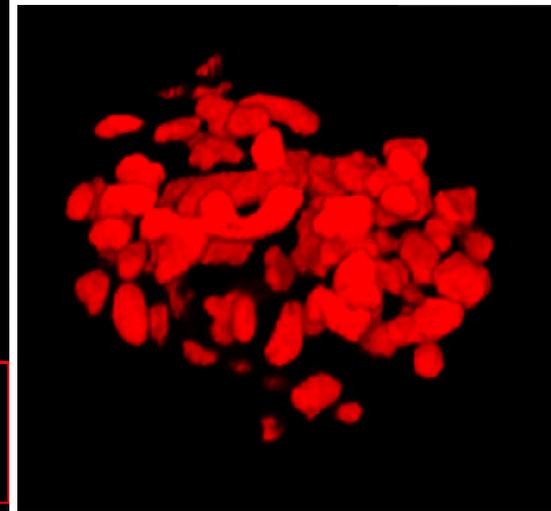
Applications of the confocal microscopy in cell therapy

3D cellular imaging

Z stack from cultured Mustem Cells

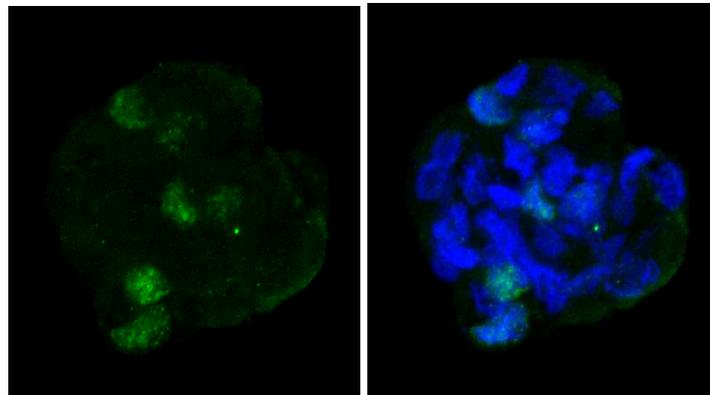


Confocal 3D imaging of cultured cells



Myosphere, Z projection

Blue : Nuclei
Green : Myod1

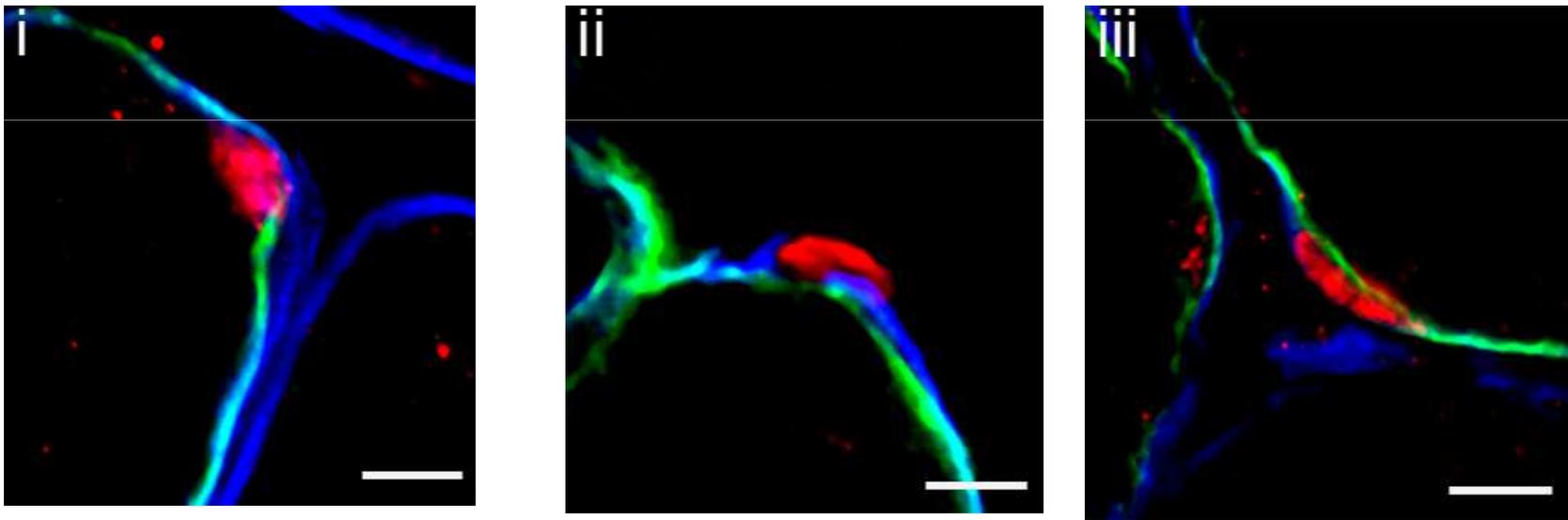


Applications of the confocal microscopy in cell therapy

Subcellular localisation

Detection of Mustems after their injection in the muscle

Muscle section, Z projection

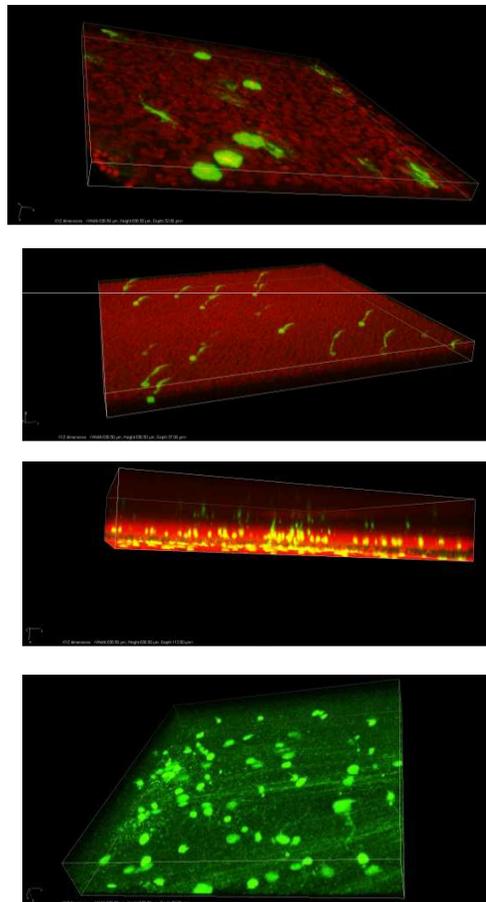


Triple immunolabeling, dystrophine (green), bgal (red), laminine(blue).

Applications of the confocal microscopy in gene therapy

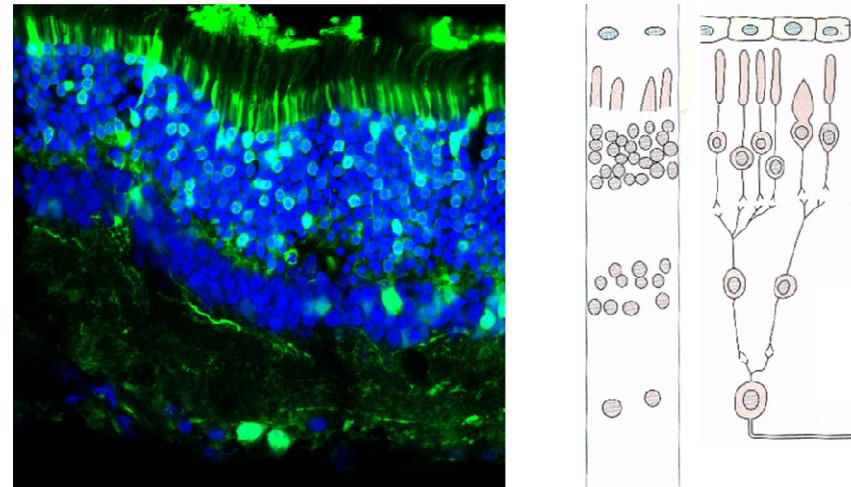
Investigation on wholemout retina

Confocal 3D imaging of retina



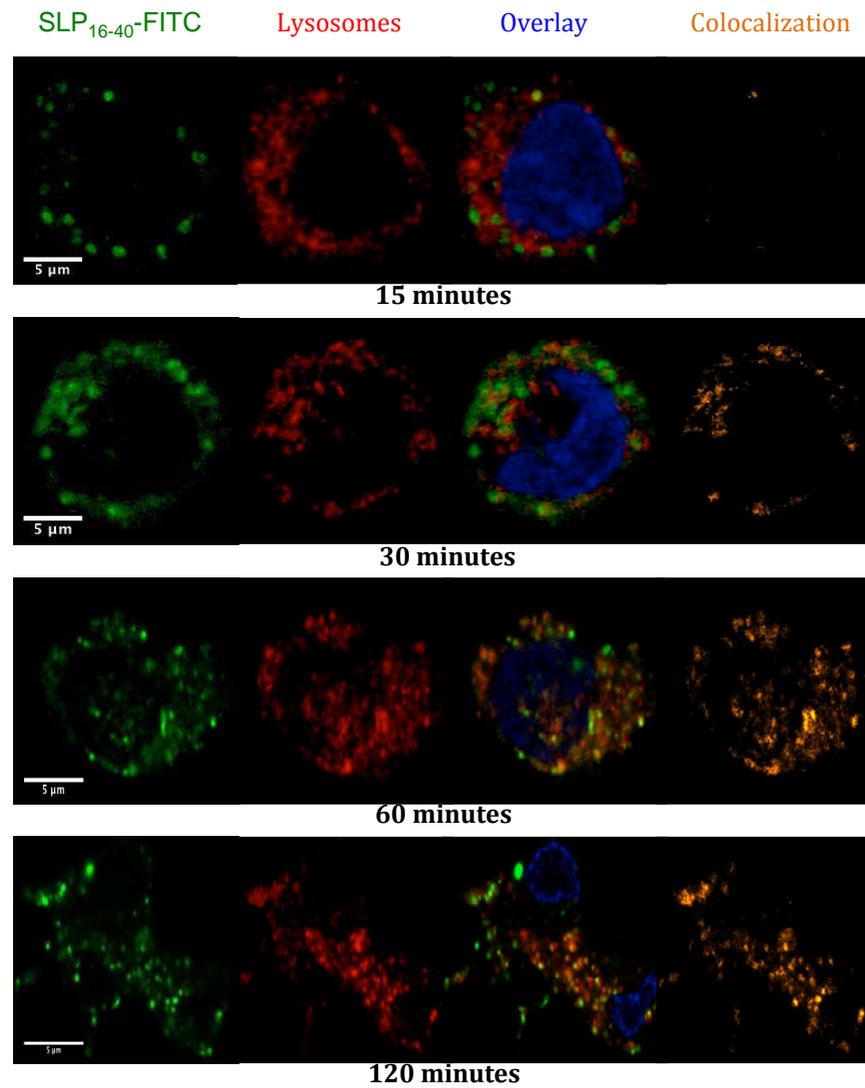
Retinal wholemout

Cartography of GFP expression in the retina after IV injection of AAV10-egfp (newborn rats)



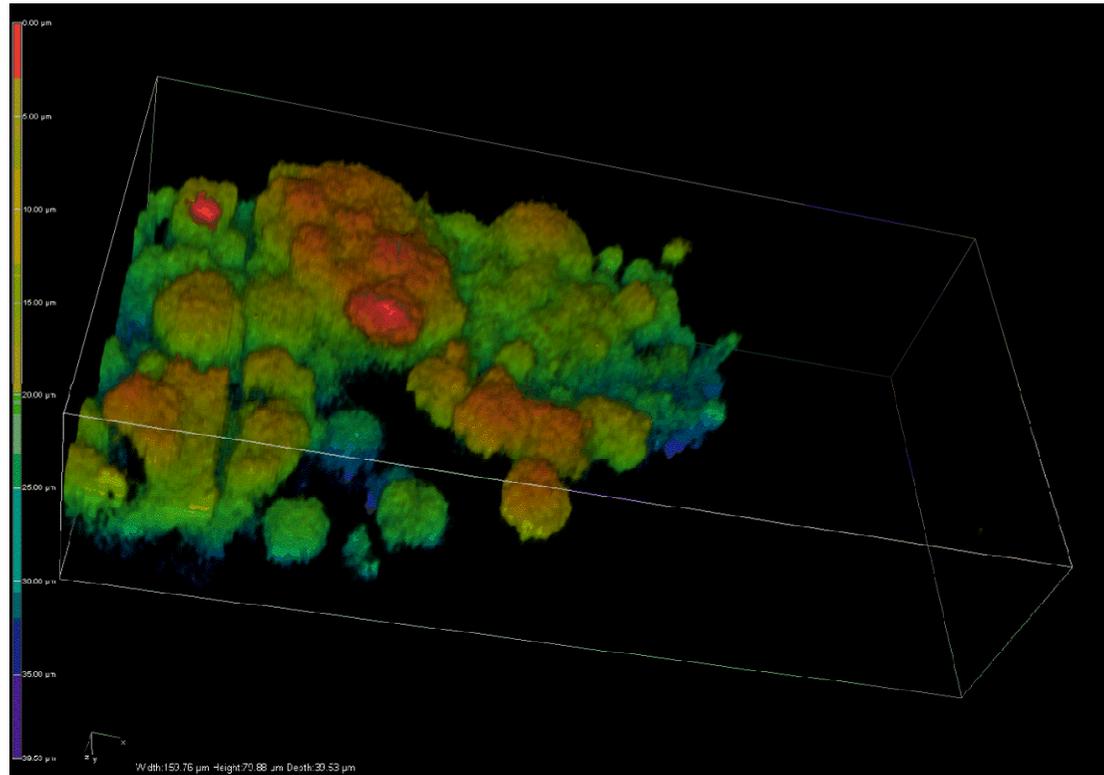
Cryosections of retina : Transduced ganglion cells are underestimated compared to the numerous transduced ganglion cells observed on retinal wholemout (non invasive method).

Applications of the confocal microscopy



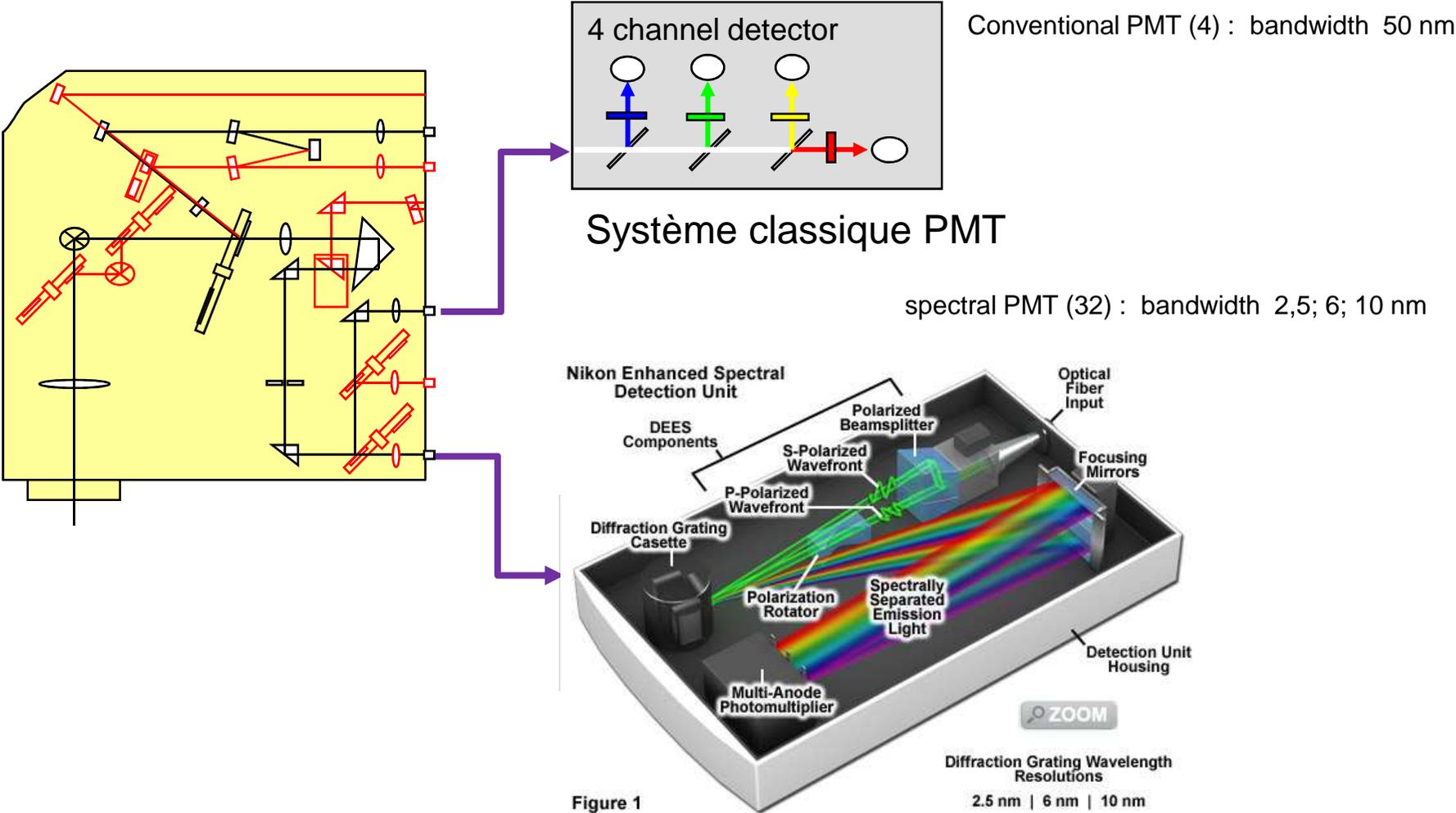
Applications of the confocal microscopy

cardiomyocytes



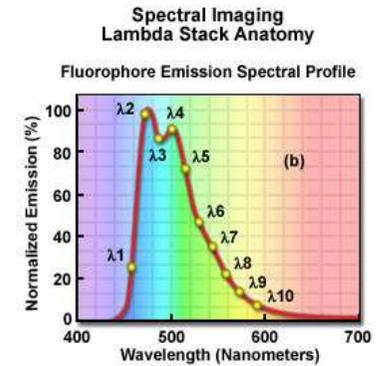
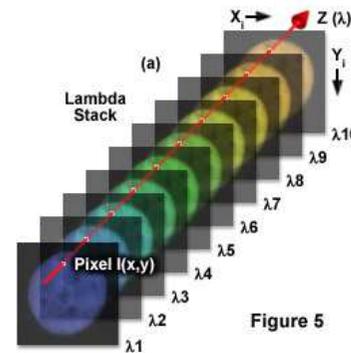
Spectral Confocal microscopy

Major input : spectral separation of emission light



Applications of spectral confocal microscopy

Major Input : specificity of signal by spectral analyses



Separation of fluorescent probe with close emission spectra

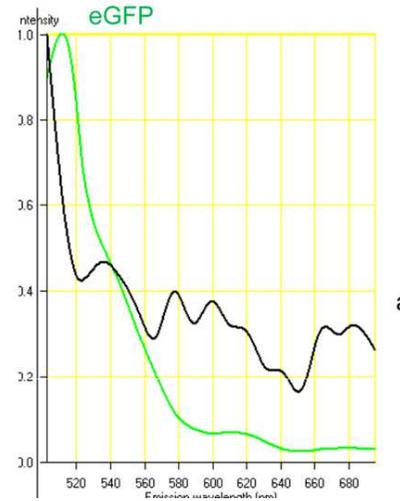
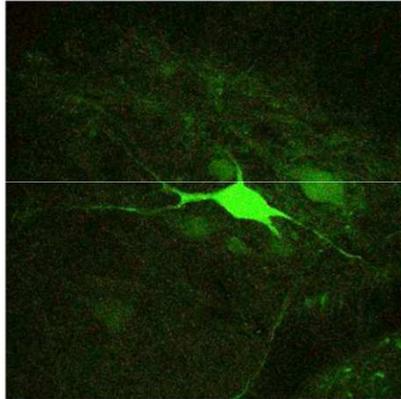
Multilabeling not limited to the 4 PMT

Studies of molecular interactions (ligand and receptor) by transfert of fluorescence (FRET)

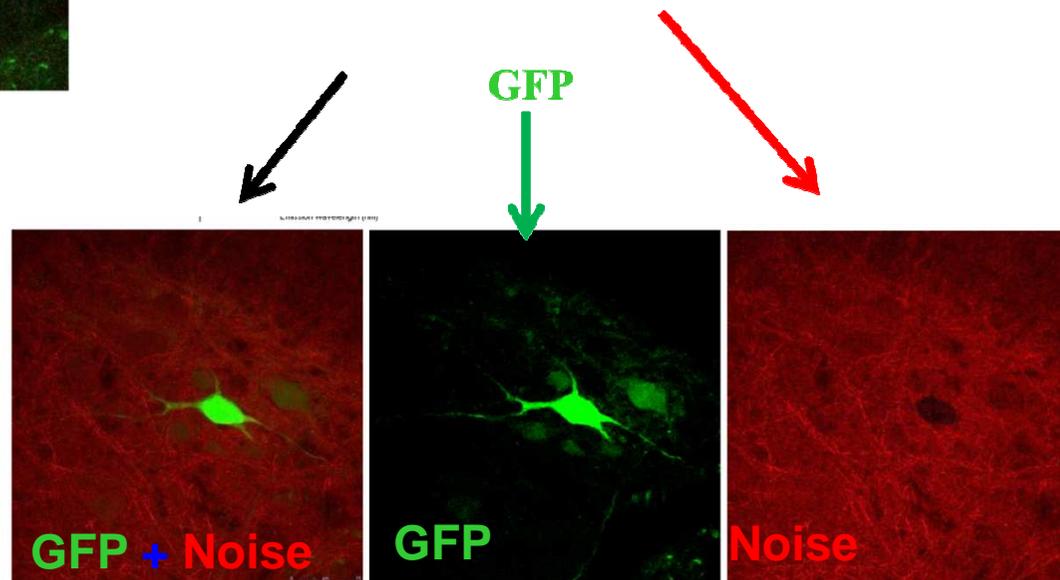
Spectral Confocal microscopy

Separation of fluorescent probe with close emission spectra

Image without unmixing

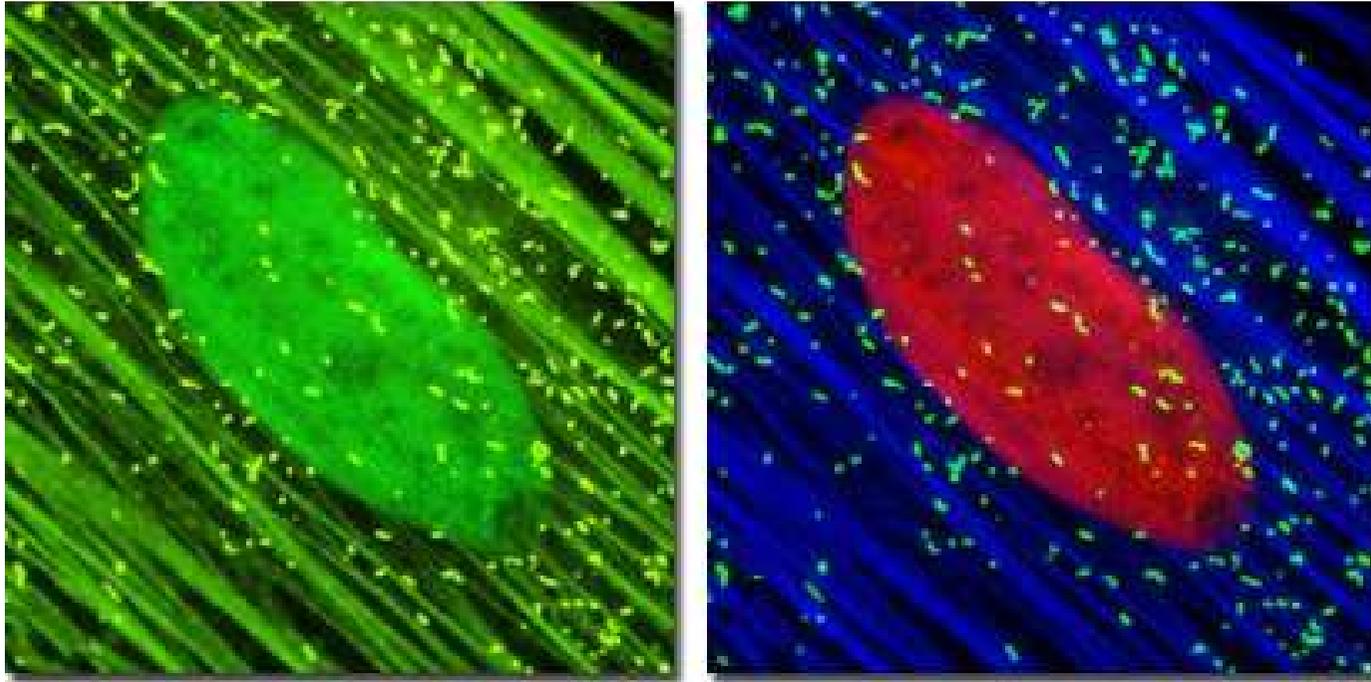


Spectral imaging and linear unmixing separate specific eGFP signal from noise (autofluorescence) generated by chemical fixation of the tissues



Spectral Confocal microscopy

Triple immunolabelling with green probes (P. Hulin)



Nucleus -> SYTOX Green (noyau),
Actine -> Alexa Fluor 488
Peroxisomes -> Alexa Fluor 514

Spectral confocal microscopy



Reduction of blurring

Increasing of resolution : 30% xy ; 30% z

Increasing of signal/noise

Observation up to 100 μm (thickness of specimen)

Light source : laser ; decrease of cross talk

3D imaging

Linear unmixing

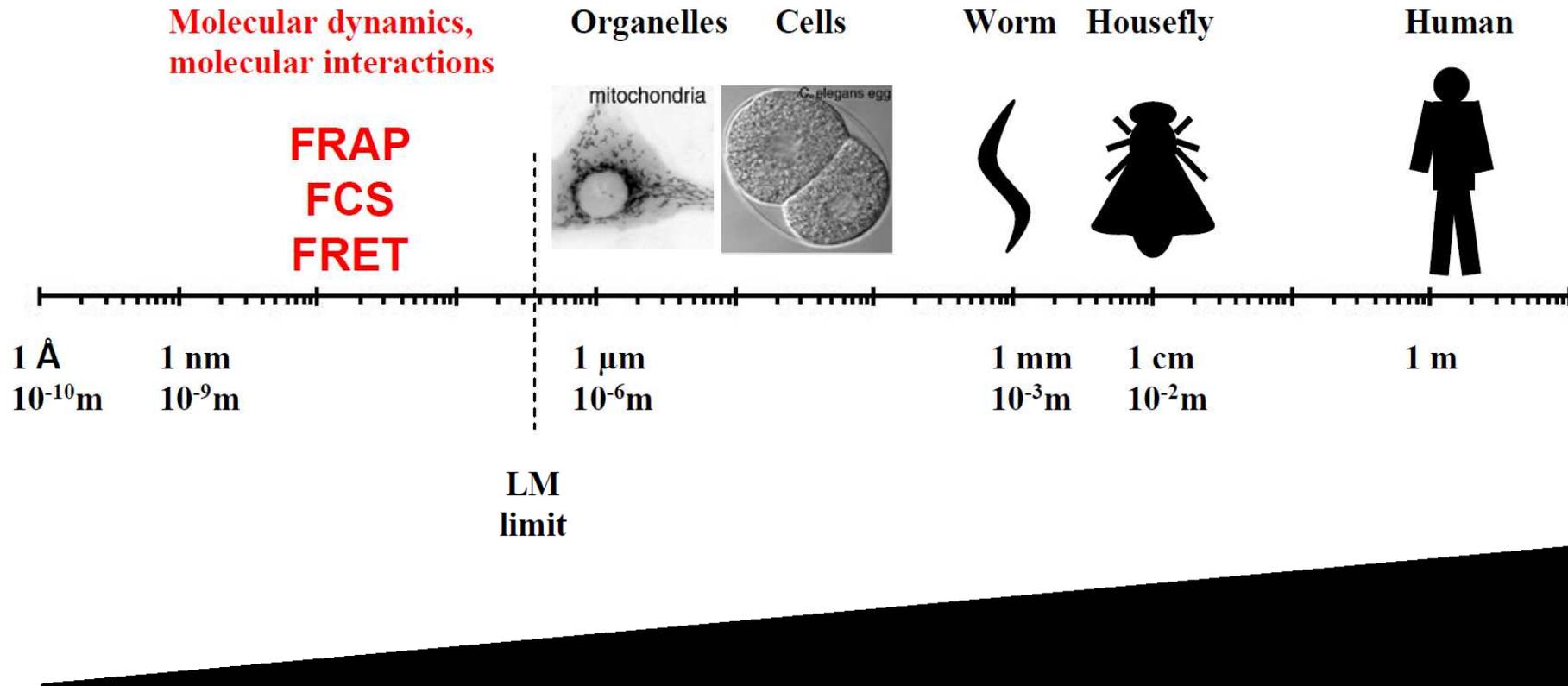


Excitation of all specimen planes,
photobleaching

Observation above 100 μm not possible
(thickness of specimen)

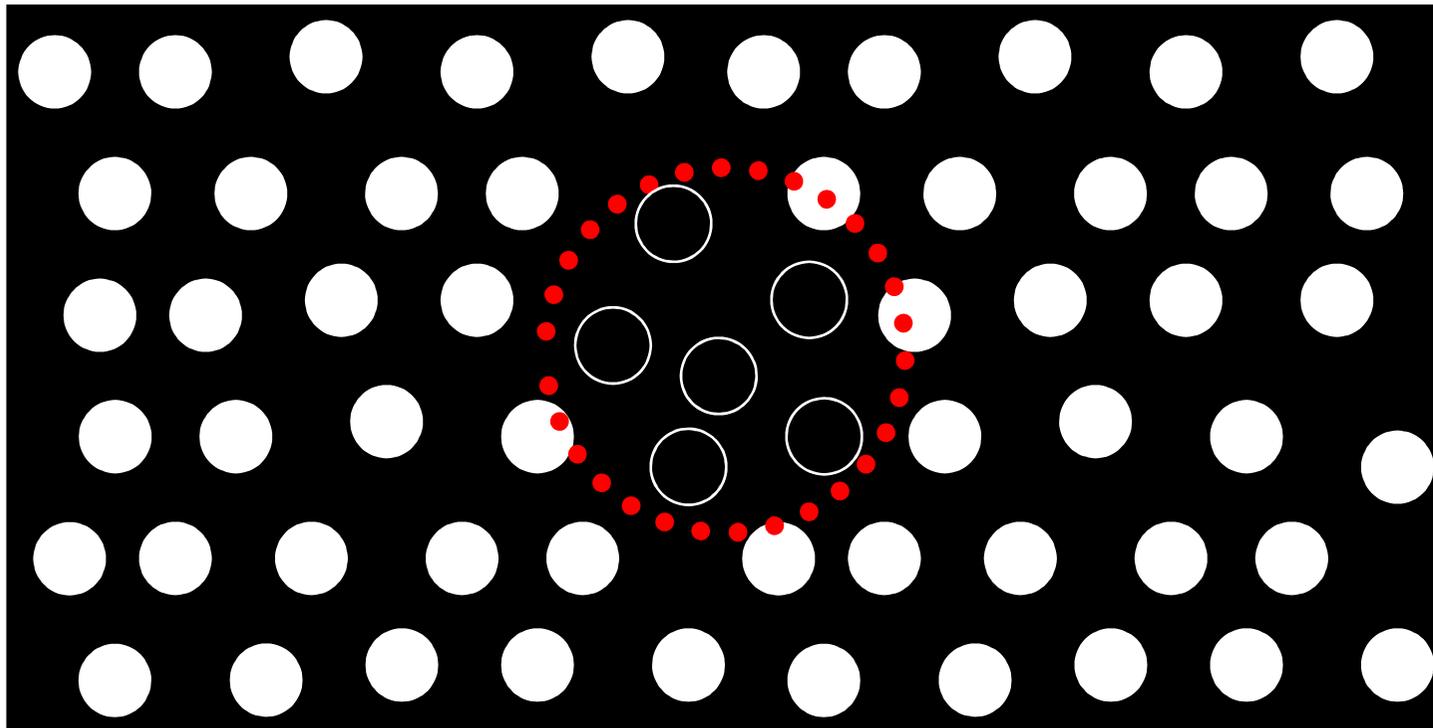
Fast acquisition : resonant scanning

« F words of kinetic microscopy: FRAP, FLIM/FRET, FCS »



Recent developments in advanced microscopy techniques, the so-called F-techniques, including Förster resonance energy transfer, fluorescence correlation spectroscopy and fluorescence lifetime imaging, have led to a wide range of novel applications in biology. The F-techniques provide quantitative information on biomolecules and their interactions and give high spatial and temporal resolution. In particular, their application to receptor protein studies has led to new insights into receptor localization, oligomerization, activation and function *in vivo*.

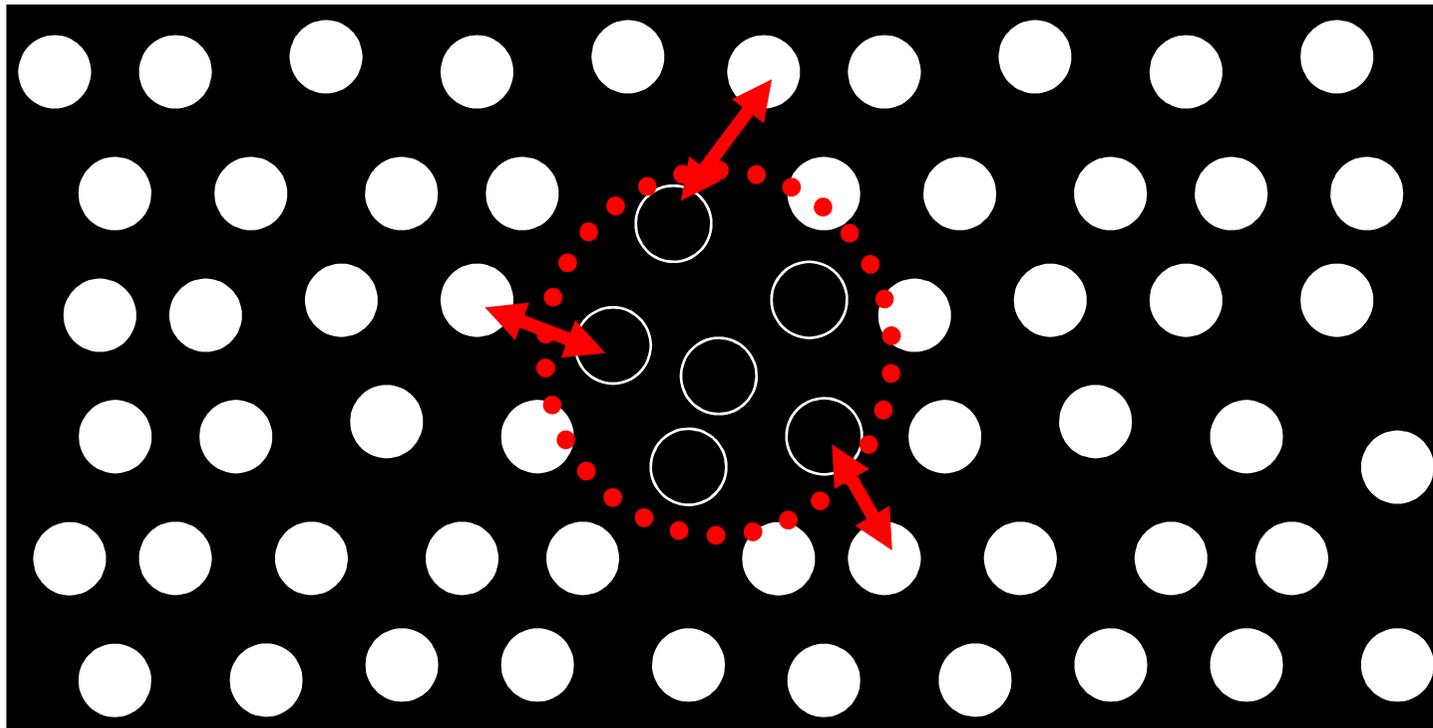
Fluorescence Recovery After Photobleaching (FRAP)



Kota Miura, EMBL Heidelberg, Germany. Based on the EAMNET Practical Course (20, April, 2004)

We think of fluorescence as a random walk. Bleached molecules (white circles) represent the molecules.

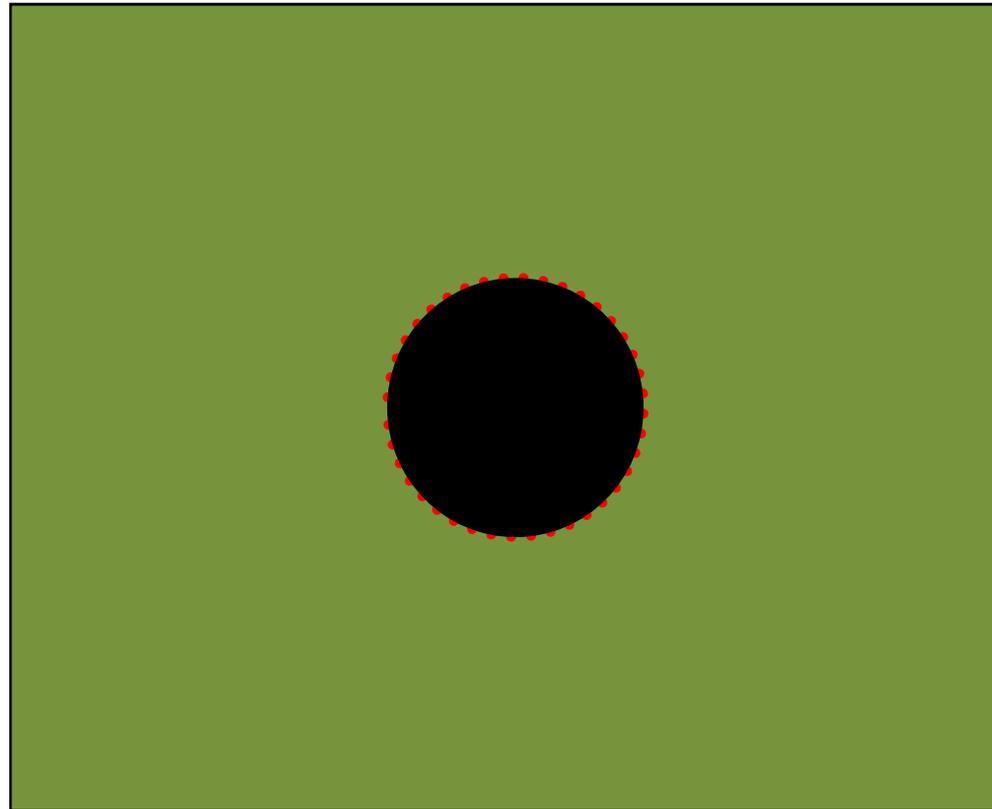
Fluorescence Recovery After Photobleaching (FRAP)



Kota Miura, EMBL Heidelberg, Germany. Based on the EAMNET Practical Course (20, April, 2004)

Since molecules are moving driven by diffusion or active transport,
Then the average intensity at the bleached spot recovers.
bleached molecules exchange their place with un-bleached molecules.

Fluorescence Recovery After Photobleaching (FRAP)

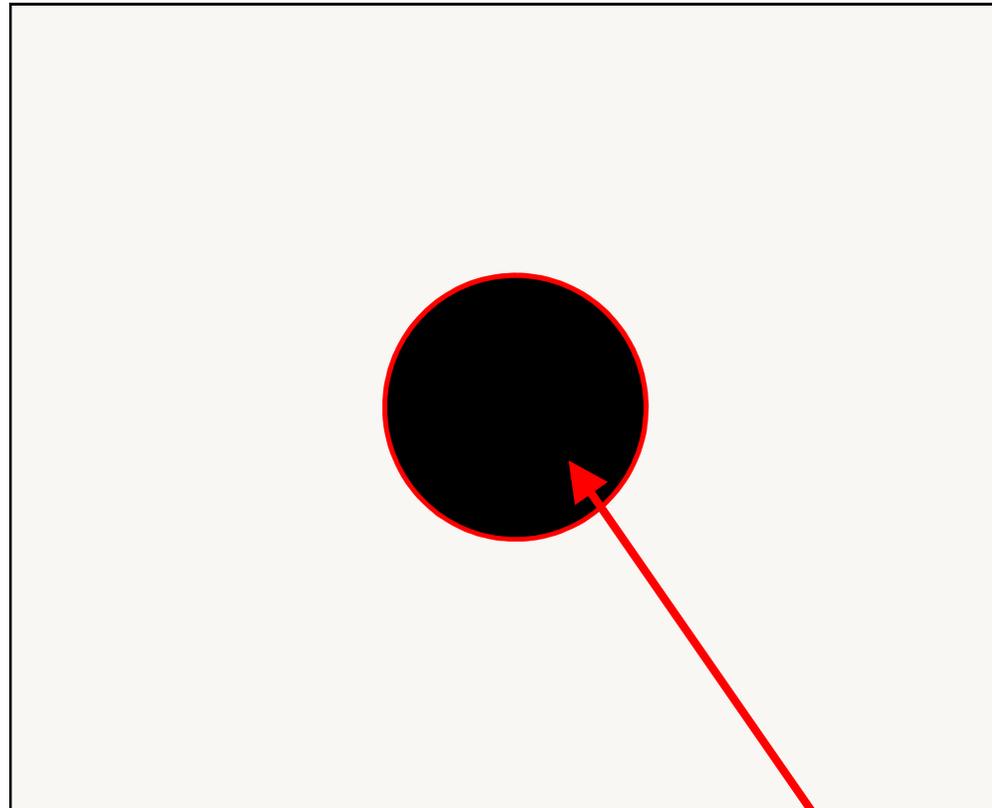


Kota Miura, EMBL Heidelberg, Germany. Based on the EAMNET Practical Course (20, April, 2004)

In practice, the FRAP at a single spot is the following. Above is a microscope field filled with fluorophores.

Fluorescence Recovery After Photobleaching (FRAP)

Quantitative Analysis of FRAP

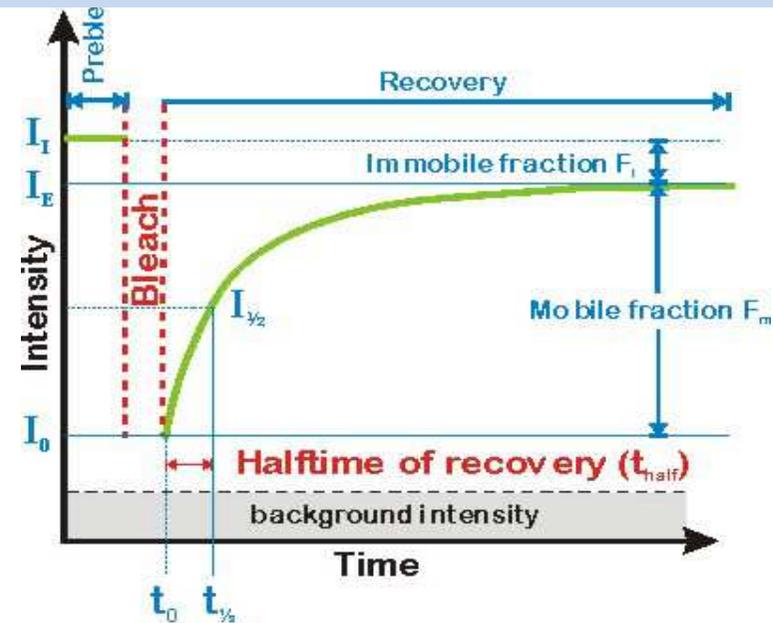
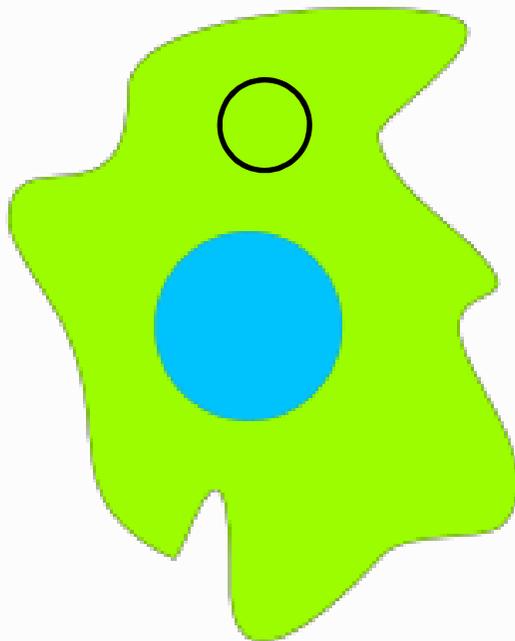
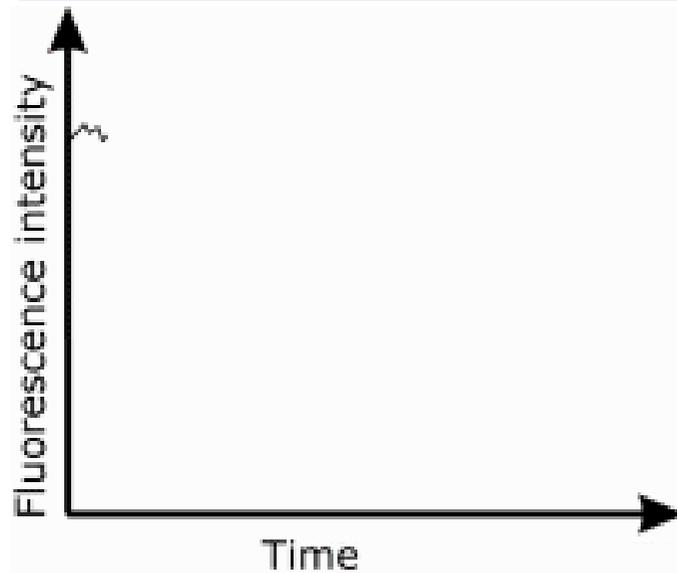


Kota Miura, EMBL Heidelberg, Germany. Based on the EAMNET Practical Course (20, April, 2004)

To gain information on molecular dynamics, time-course of the fluorescence recovery must be measured.

Measure the temporal changes of the fluorescence Intensity!

Fluorescence Recovery After Photobleaching (FRAP)



An idealized plot of a FRAP recovery curve.

I_i : initial intensity

I_0 : intensity at timepoint t_0 (first postbleach intensity)

$I_{1/2}$: half recovered intensity ($I_{1/2} = (I_E - I_0) / 2$)

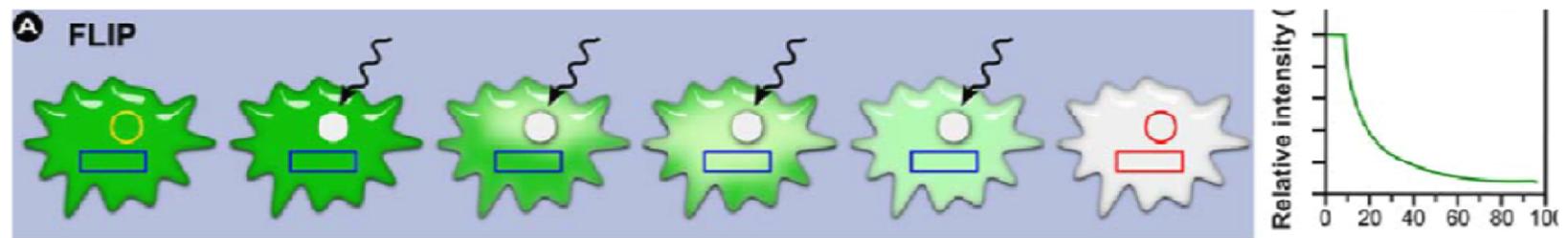
I_E : endvalue of the recovered intensity

t_{half} : Halftime of recovery corresponding to $I_{1/2}$ ($t_{1/2} - t_0$)

Mobile fraction $F_m = (I_E - I_0) / (I_i - I_0)$

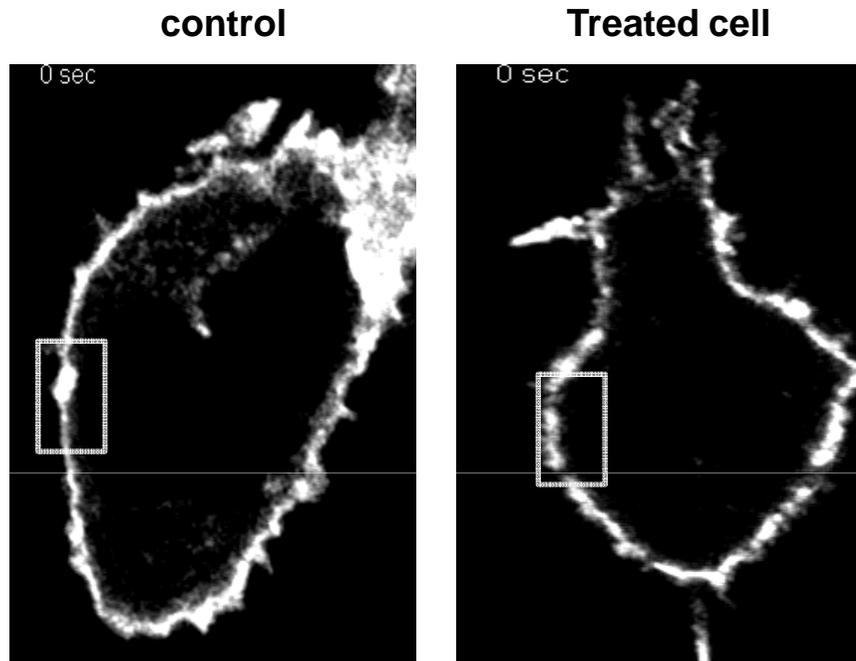
Immobile fraction $F_i = 1 - F_m$

Fluorescence Recovery After Photobleaching

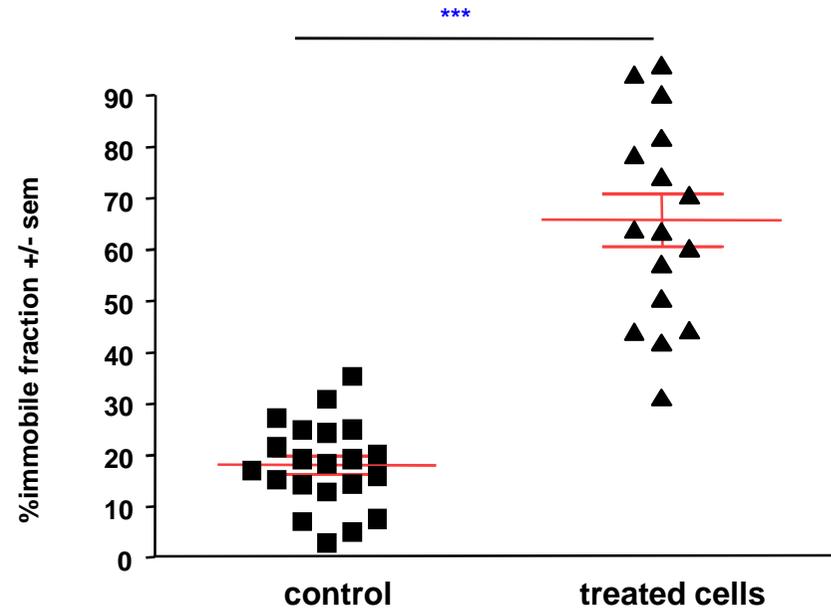


FLIP (fluorescence loss in photobleaching). In this technique, an area within the cell is repeatedly bleached and the loss of fluorescence in areas that are distant from the bleach area is monitored. The decline in fluorescence intensity in the surrounding regions is due to bleaching of fluorochromes that move through the ROI during the repetitive bleaching process.

Fluorescence Recovery After Photobleaching

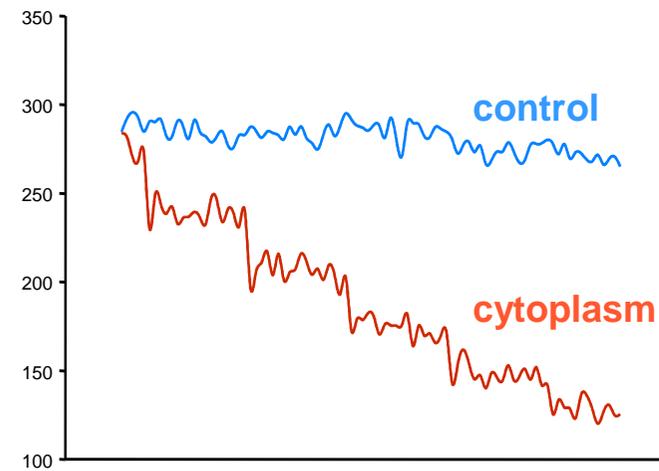
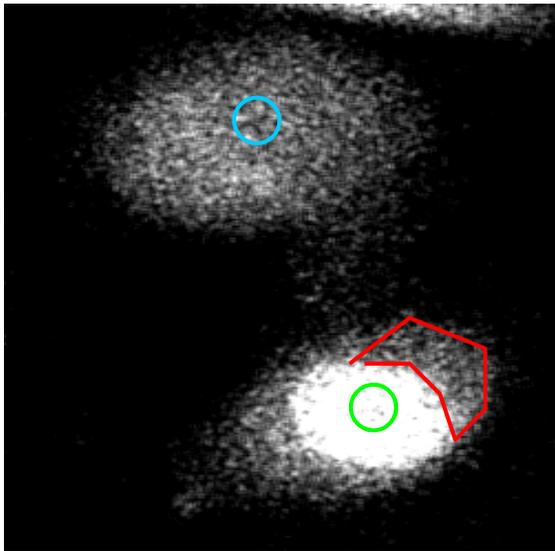


Monitored cells were transduced to express a fusion GFP-CD277 butyrophilin molecule



Control and treated cells display different patterns of GFP tagged protein membrane mobility.

Fluorescence Loss In Photobleaching (FLIP)

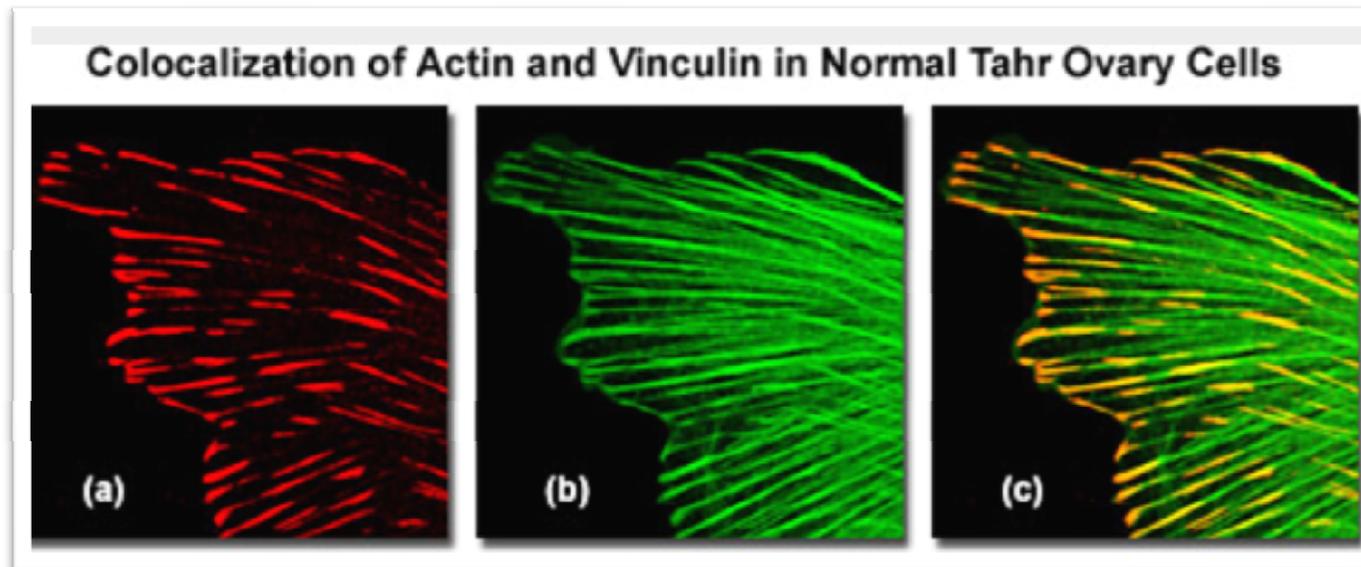


Fluorescence Recovery After Photobleaching

Recapitulating, FRAP is generally suitable to study and investigate:

- Protein/molecule movement and diffusion (diffusional speed).
- Compartmentalization and connections between intracellular compartments.
- The speed of protein/molecule exchange between compartments (exchange speed).
- Binding characteristics between proteins. Additionally, the effect of mutations that alter individual amino acids on protein association, and the effect of small molecules, such as drugs or inhibitors, on protein pairs can effectively be studied using FRAP.
- Immobilization of proteins that bind to large structures, e.g., DNA, nuclear envelope, membranes, cytoskeletal elements, etc

Forster Resonant Energy Transfert (FRET) / Fluorescence Lifetime Imaging (FLIM): supplying co-localization

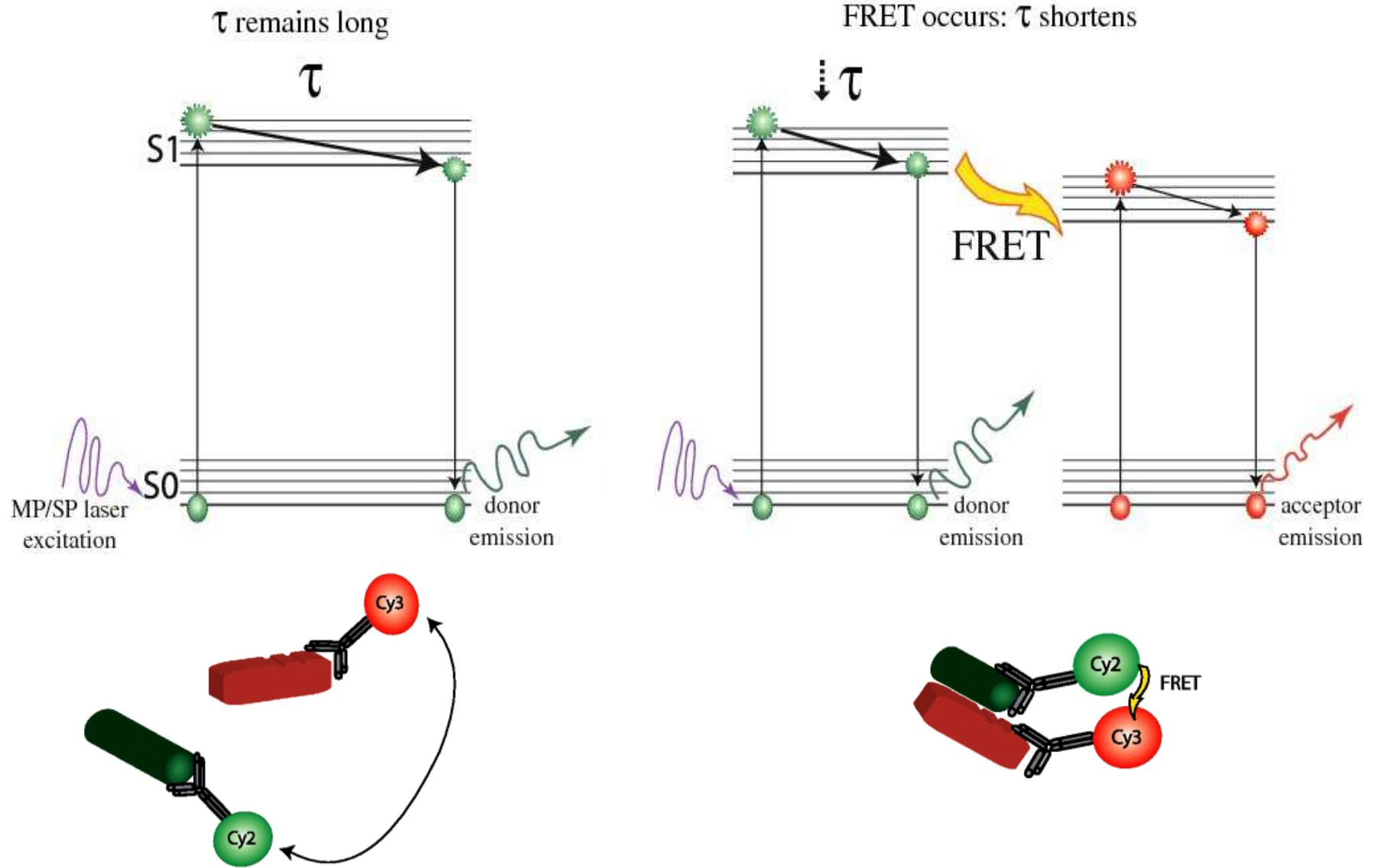


olympusconfocal.com

Colocalization, in a biological manifestation, is defined by the presence of two or more different molecules residing at the same physical location in a specimen. Overlay of both channels (red and green) displays a strong colocalization viewable in yellow.

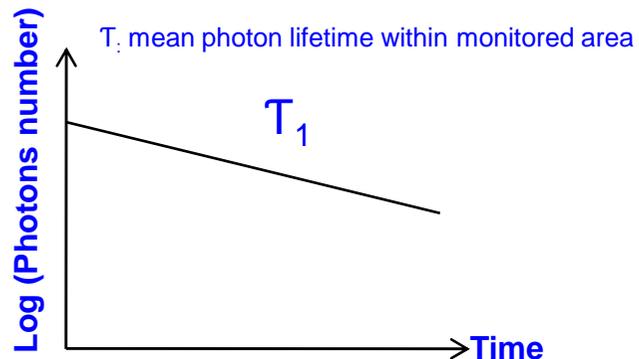
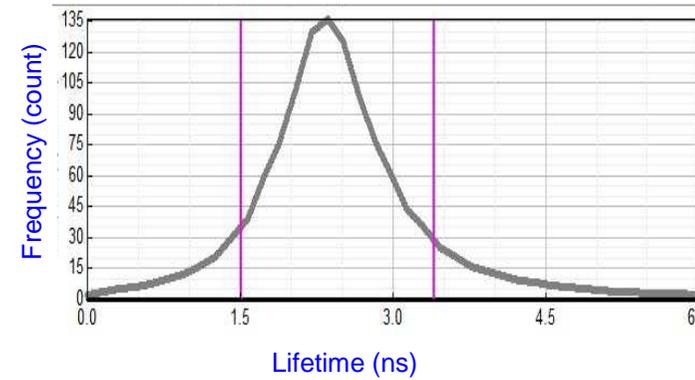
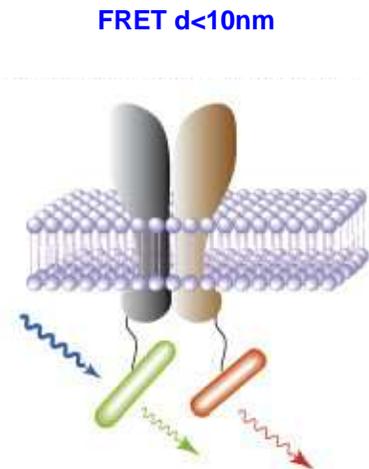
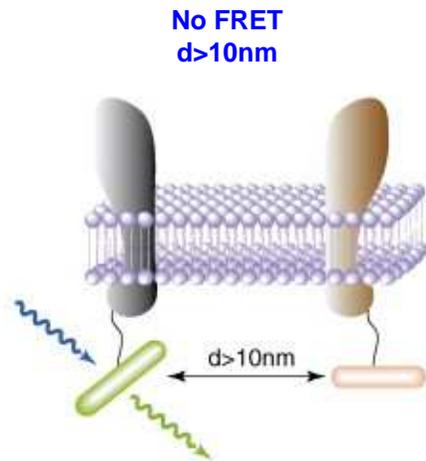
The ability to determine colocalization in a confocal microscope is limited by the resolution of the optical system and the wavelength of light used to illuminate the specimen. Widefield fluorescence and confocal microscopes have a theoretical resolution of approximately 200 nanometers

FLIM/FRET: supplying co-localization

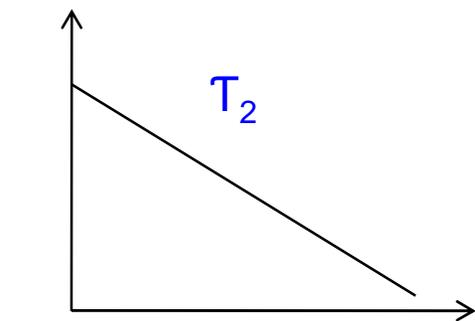


FLIM/FRET: supplying co-localization

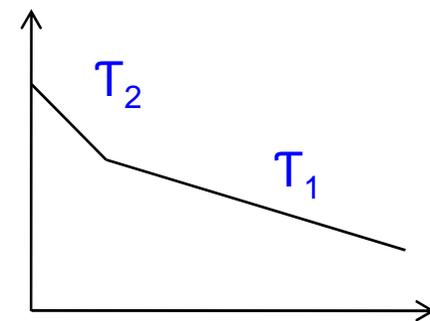
FLIM (Fluorescence Lifetime Imaging Microscopy) is a powerful technique to measure protein-protein interactions, and is based on the FRET (Förster Resonant Energy Transfer) principle, as shown below.



Mono exponential decline:
100% No FRET
(negative control condition)

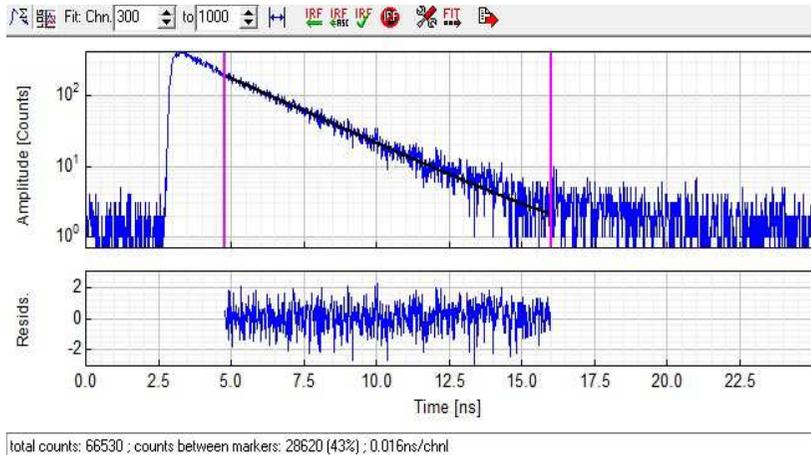


Mono exponential decline:
100% FRET (shorten lifetime)
(positive control condition)



Bi-exponential decline:
33% FRET (T_2)
66% No FRET (T_1)

FLIM/FRET: supplying co-localization

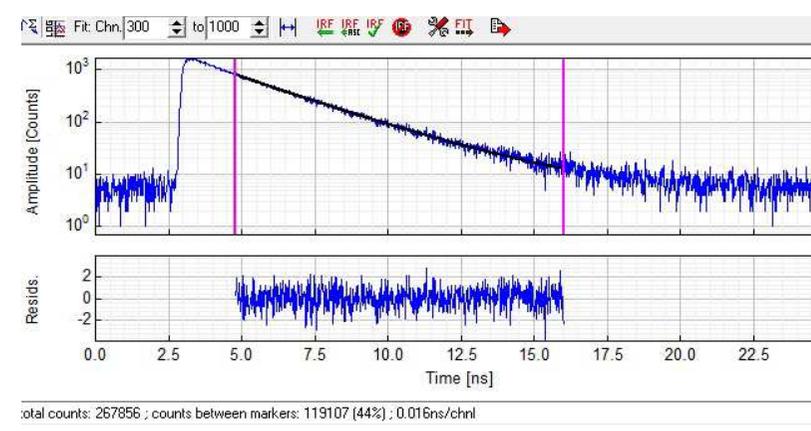
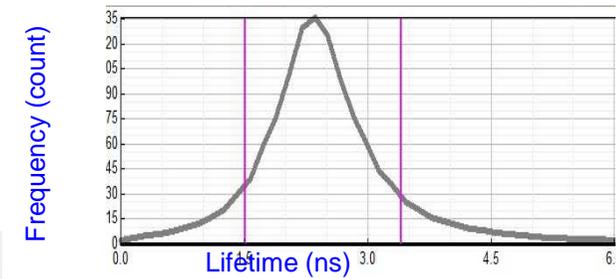
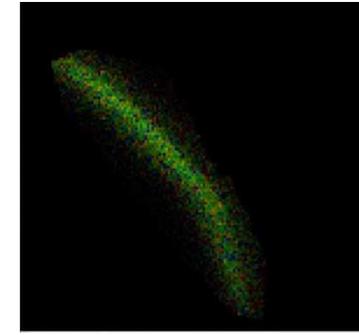


Mono-exponential fitting

Exp.: 1

Ampl. 1	189.68
Lifet. 1	2.349
Backgr.	0.46

χ^2 : 0.819 || τ_{amp} : 2.35 ns || τ_{int} : 2.35 ns

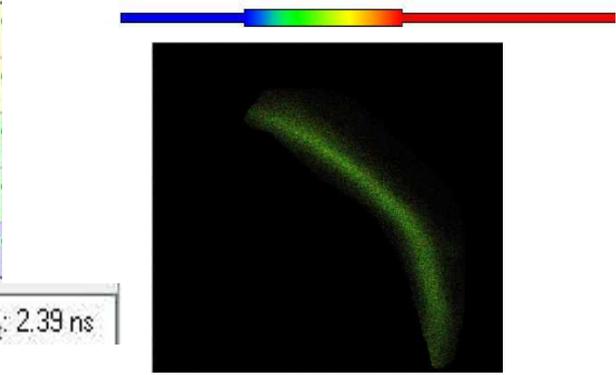


Bi-exponential fitting

Exp.: 2

Ampl. 1	113.83
Lifet. 1	1.23
Ampl. 2	687.3
Lifet. 2	2.483
Backgr.	5.39

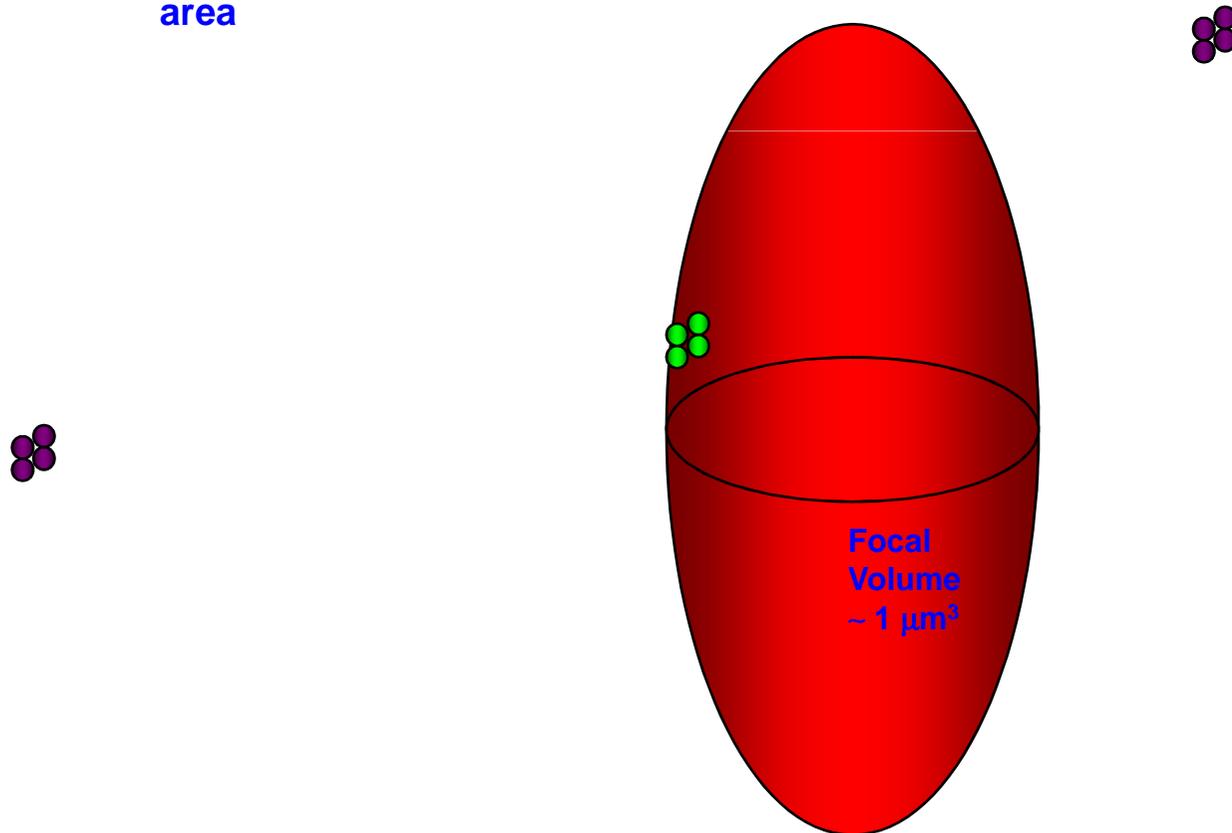
χ^2 : 0.973 || τ_{amp} : 2.31 ns || τ_{int} : 2.39 ns



Fluorescent Correlation Spectroscopy

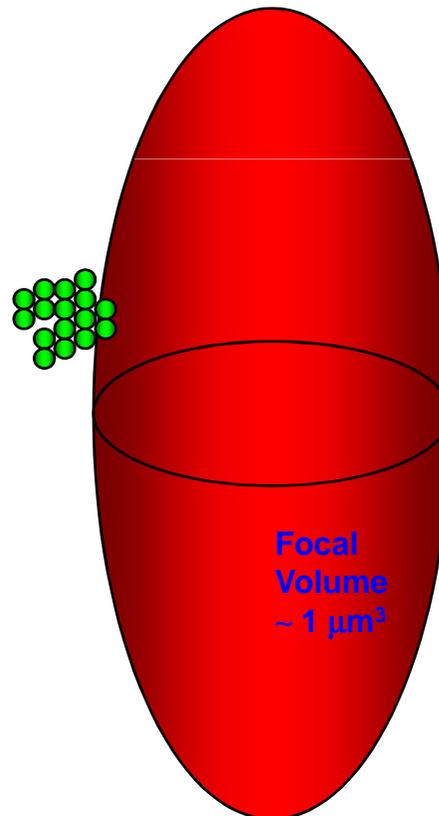
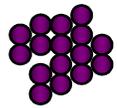
FCS (fluorescence correlation spectroscopy) provides an alternative method for measurements of protein dynamics *in vivo*. A laser beam is focused on a microvolume, typically in the femtolitre range, and fluctuation of the fluorescence signal is measured over a short period of time. The recorded signals reflect the movement of labelled proteins through the sample volume

Fast Dynamics
Short lifetime
inside spotted
area

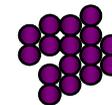


Fluorescent Correlation Spectroscopy

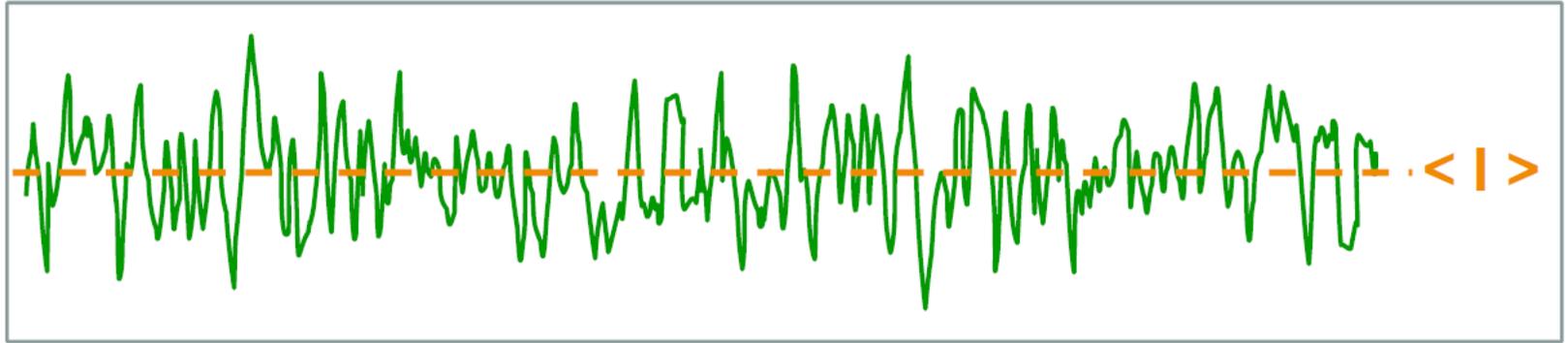
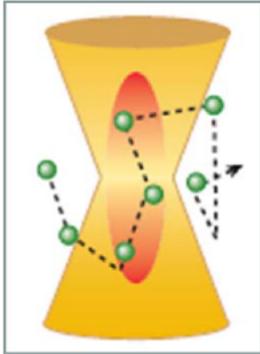
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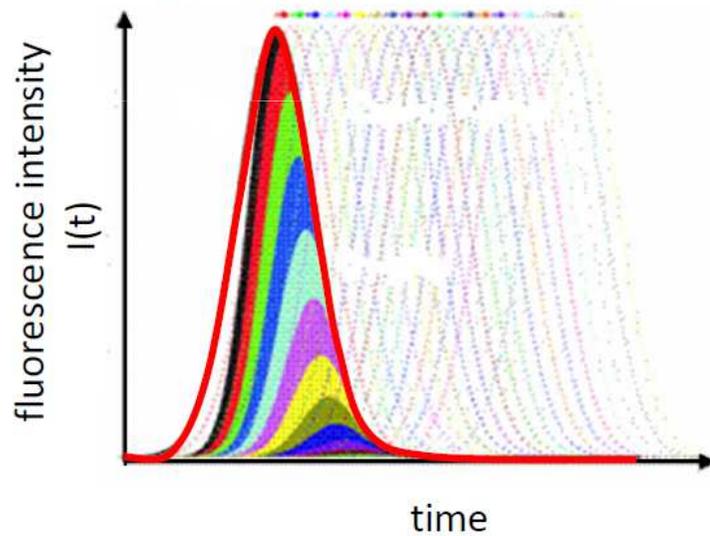
**Slow Dynamics
Long lifetime
inside spotted
area**



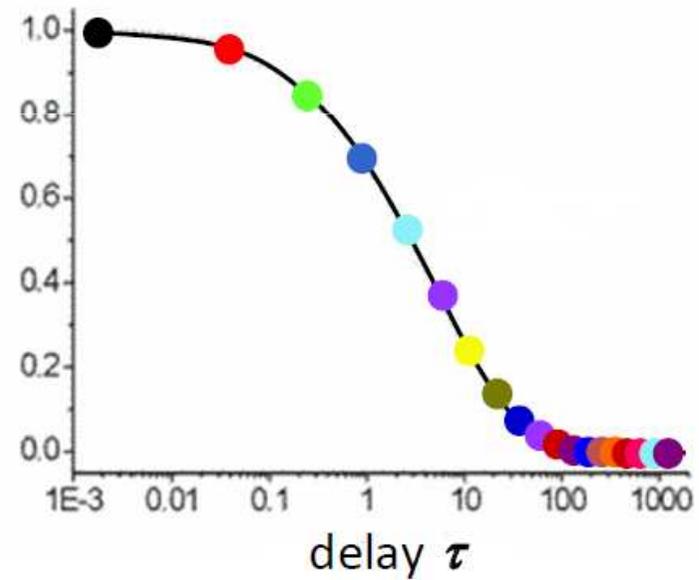
Fluorescent Correlation Spectroscopy



fluorescence fluctuation



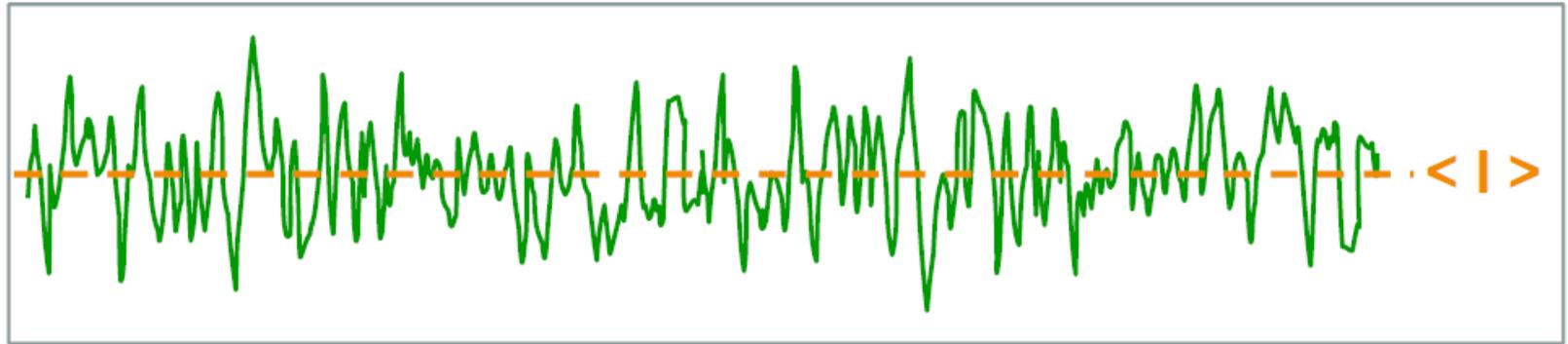
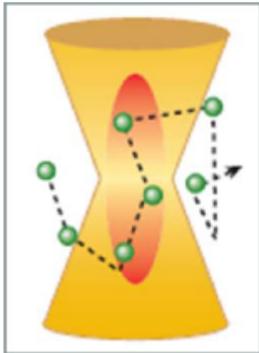
overlapping surface



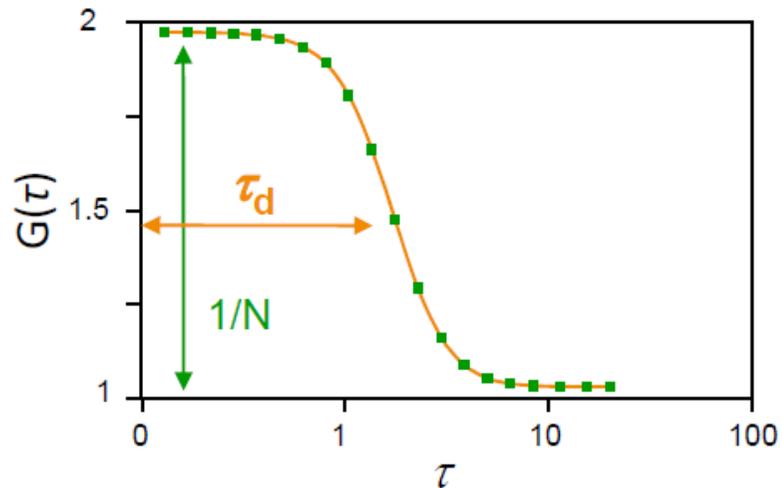
autocorrelation function

$$g^{(2)}(\tau) = \frac{\langle I(t) I(t+\tau) \rangle}{\langle I(t) \rangle^2}$$

Fluorescent Correlation Spectroscopy



temporal fluctuations

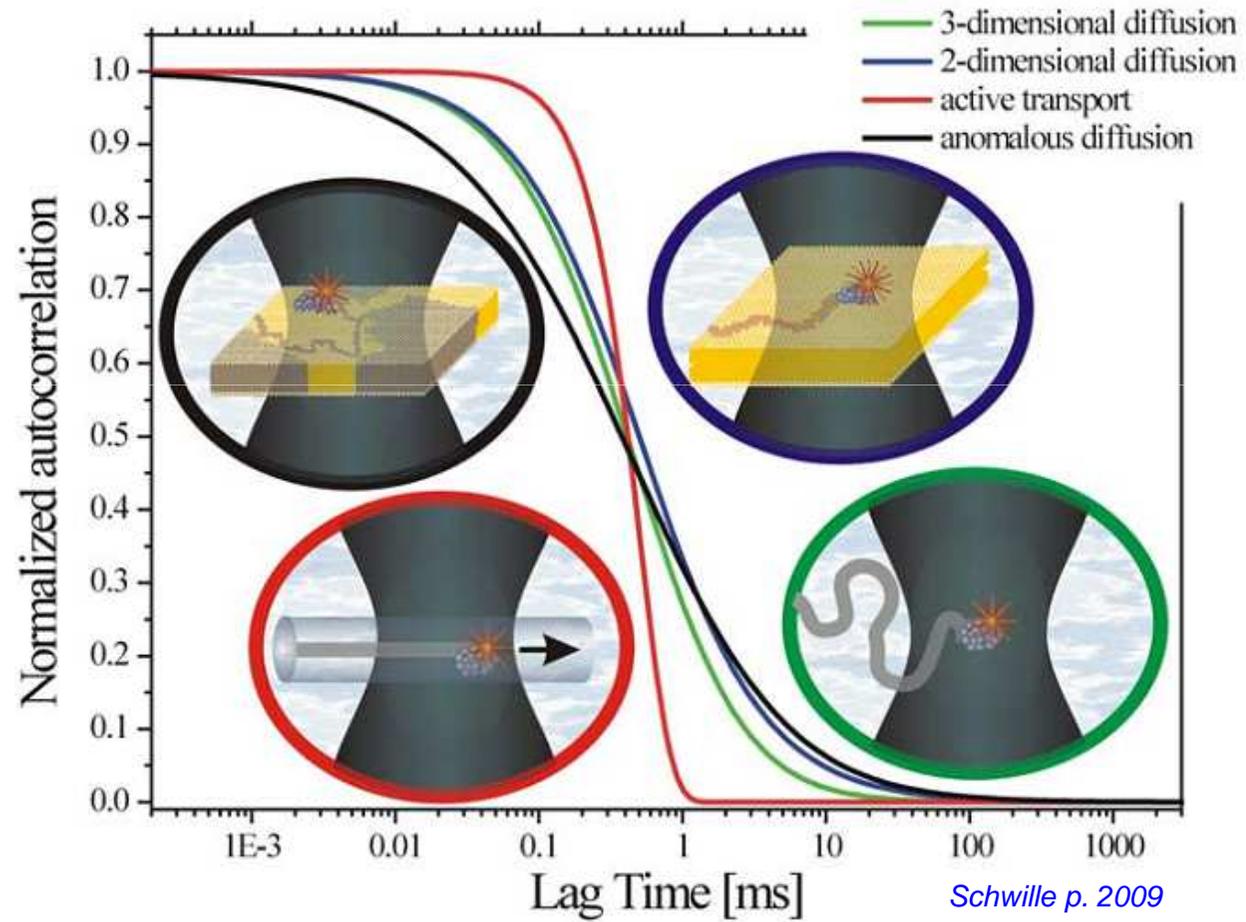


autocorrelation function (ACF)

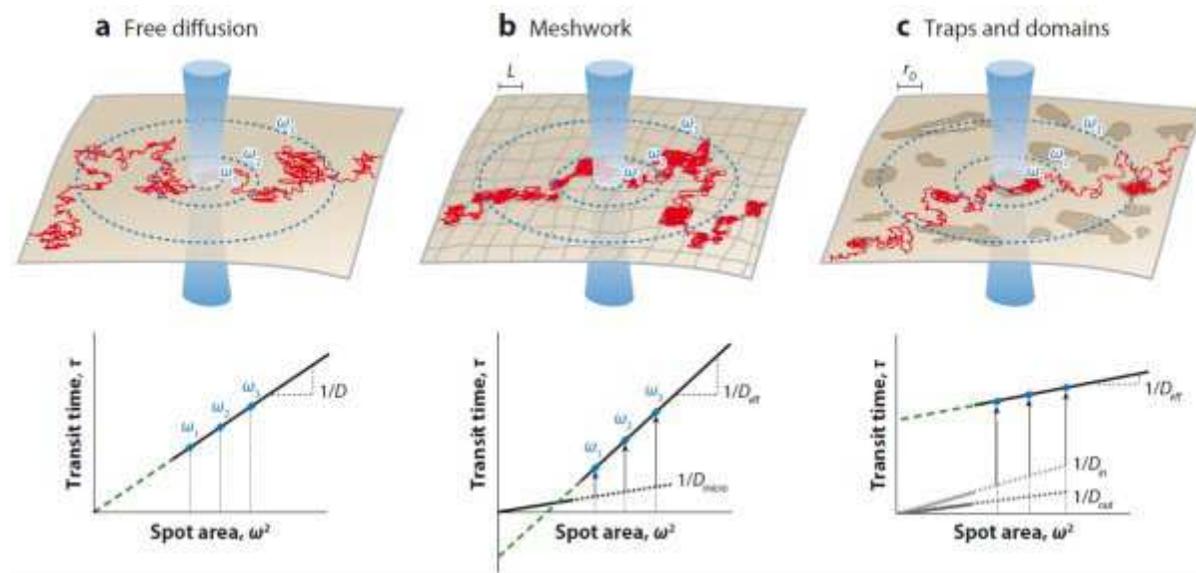
$\Rightarrow \tau_d$ the average time molecules stay within the spot

$\Rightarrow N$ the average number of molecules

Fluorescent Correlation Spectroscopy



Fluorescent Correlation Spectroscopy



Research question	Live-cell imaging	Fixed-cell imaging
Molecular structure	No	Crystallography, electron microscopy
Conformational changes	FRET, single-molecule FRET	Crystallography, electron microscopy
Mobility of bound species	FRAP, FCCS, SPT	No
Intracellular activity of proteins	FRET sensors, FRET	No
Intracellular localization	Confocal microscopy, STED microscopy	Confocal microscopy, STED microscopy, SIM, PALM
Aggregation state of receptors	Anisotropy, FRET, PALM, STORM, FCCS and related analyses of molecular brightness	TEM, PALM, STORM, FRET
Mobility at the plasma membrane	TIRF microscopy, FRAP, SPT and sptPALM, confocal microscopy, STED microscopy	No
Cell morphology	Confocal microscopy, epifluorescence microscopy, TIRF microscopy, DIC microscopy	Confocal microscopy, epifluorescence microscopy, TIRF microscopy, DIC microscopy
Cell adherence to a surface	TIRF microscopy, DIC microscopy, IRM	TIRF microscopy, DIC microscopy, IRM, TEM

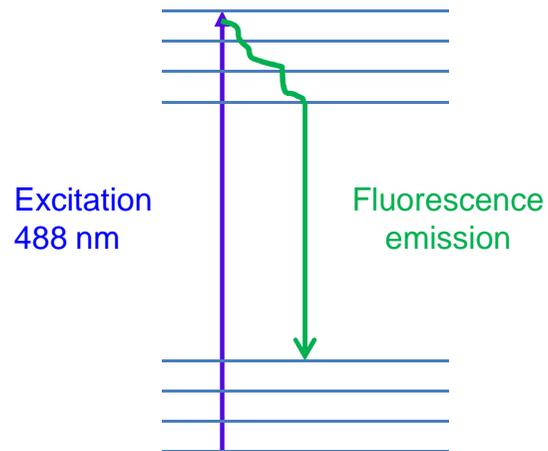
DIC, differential interference contrast; FCCS, fluorescence cross-correlation spectroscopy; FRAP, fluorescence recovery after photobleaching; FRET, fluorescent resonance energy transfer; IRM, interference reflection microscopy; PALM, photoactivated localization microscopy; SIM, structured illumination microscopy; SPT, single-particle tracking; STED, stimulated emission depletion; STORM, stochastic optical reconstruction microscopy; TEM, transmission electron microscopy; TIRF, total internal reflection fluorescence.

Biphotonic microscopy

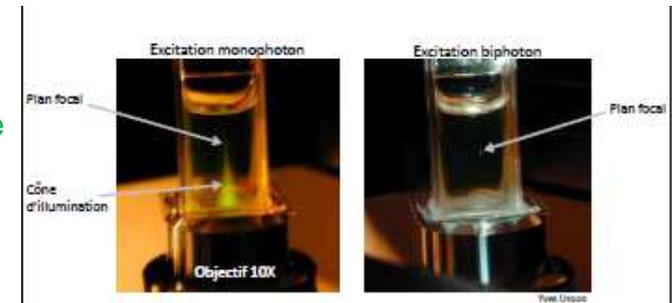
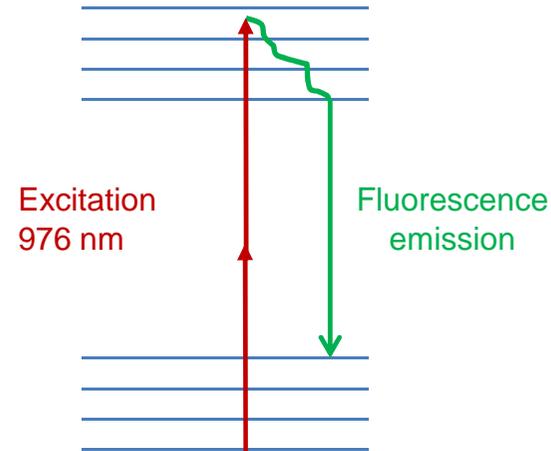
Major Inputs of 2Photon excitation:

- Deeper tissue penetration
- Reduction of the phototoxicity
- Imaging of living tissue
- Studies of FRET by FLIM
- Imaging of second harmonic signals

1Photon excitation



2Photon excitation



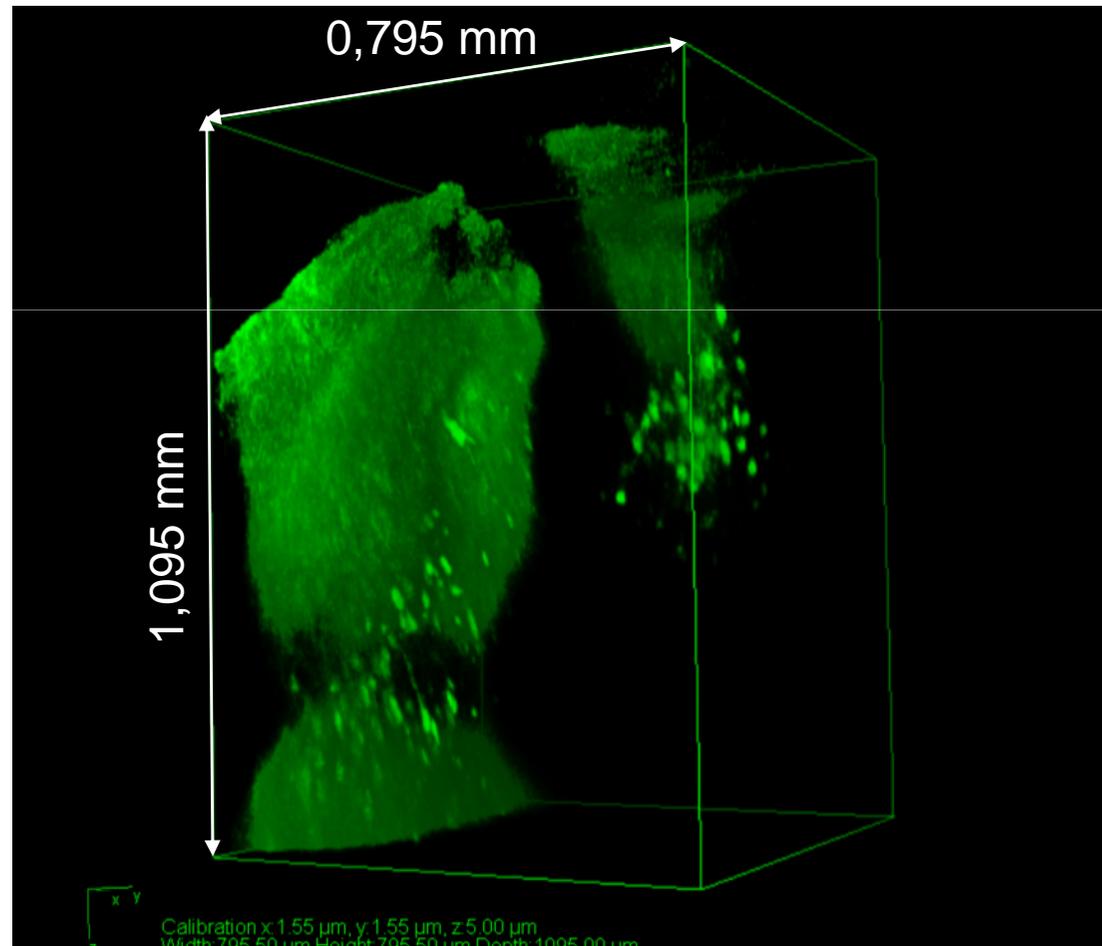
Femtosecond laser (infrared laser beam 680-1080 nm)

Applications of the biphotonic microscopy

Major Input : deeper tissu penetration (2X with biphotonic microscopy)

Scaled brain GFP expression

A1RPM, Nikon, MiFoBio 2012



Applications of the biphotonic microscopy

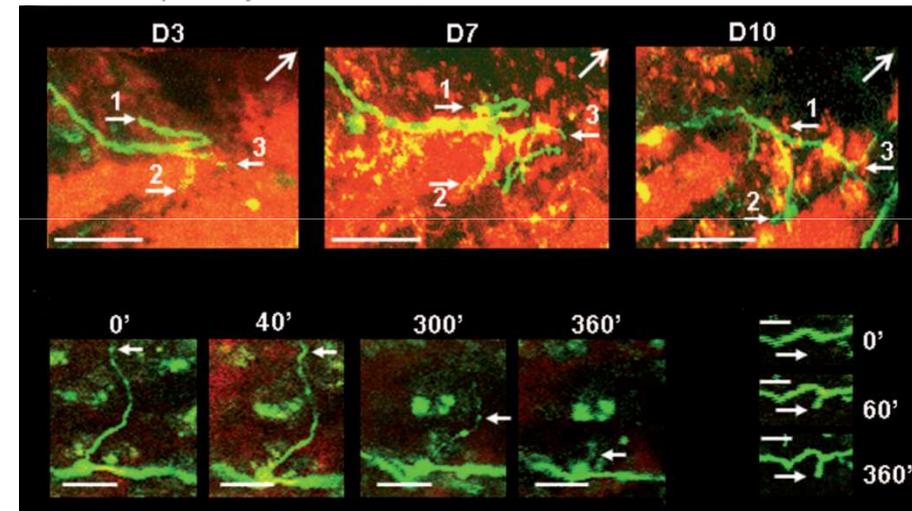
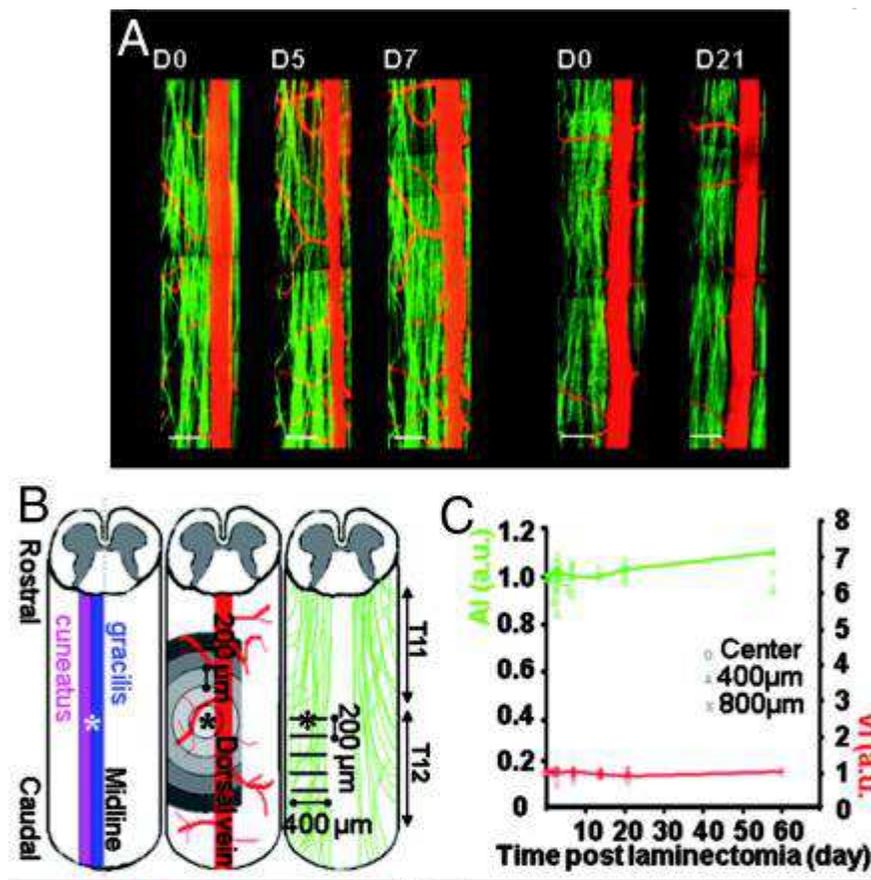
Major input : Imaging of living tissue

PNAS June 9, 2009 vol. 106 no. 23 9459–9464

Quantitative analysis by in vivo imaging of the dynamics of vascular and axonal networks in injured mouse spinal cord

Cyril Dray, Geneviève Rougon¹, and Franck Debarbieux

Unité Mixte de Recherche 6216, Centre National de la Recherche Scientifique, Université de la Méditerranée, Institut de Biologie du Développement de Marseille-Luminy, Case 907, Parc Scientifique de Luminy, 13288 Marseille Cedex 9, France

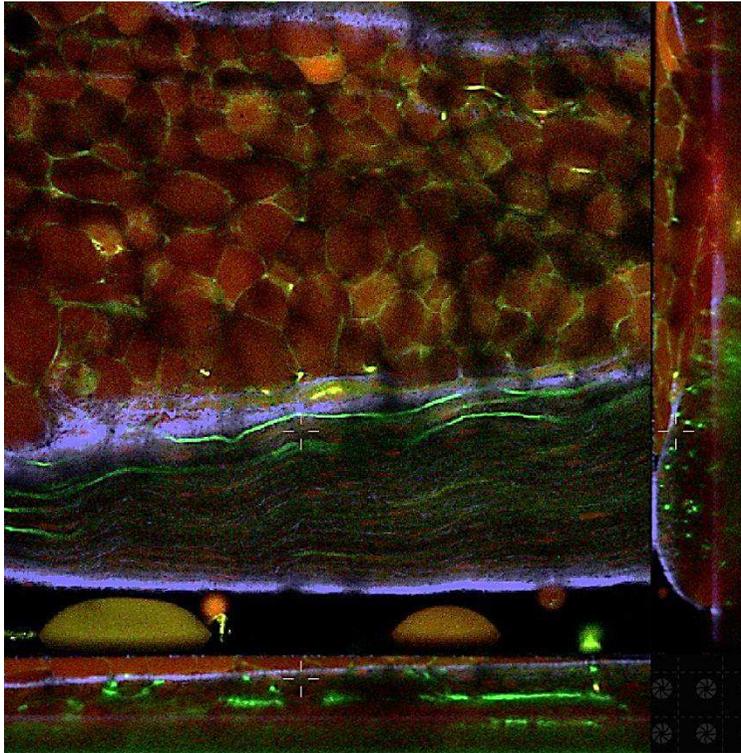


Adult transgenic Thy1GFP-M mice
Rhodamin B isothiocyanate-Dextran

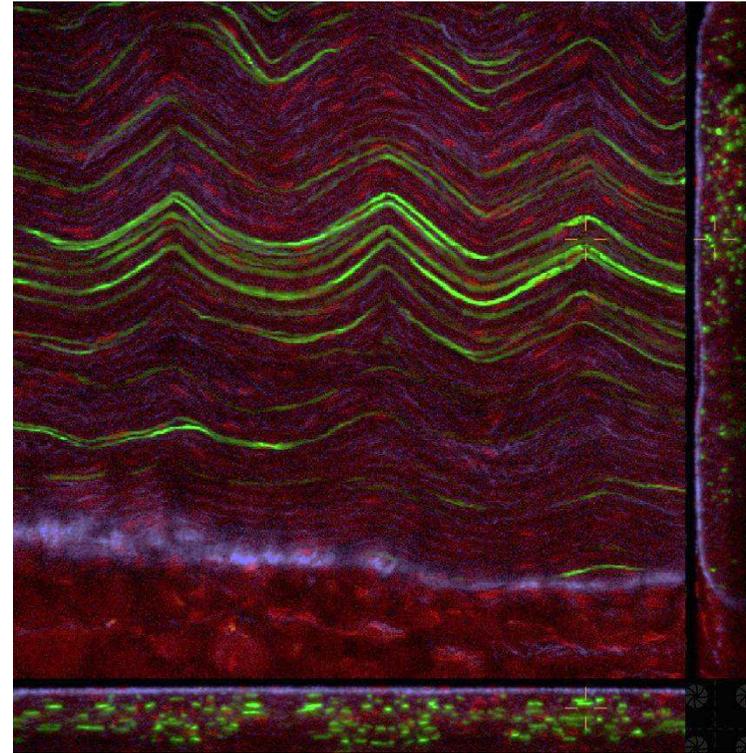
Biphotonic microscopy

Major input : second harmonic generation signal ($\lambda/2$), molecular conformation and orientation (fibrillar collagen).

sciatic nerve from a mice



A1RPM, Nikon, MiFoBio 2012



Collagen matrix : second harmonic generation

Applications of the biphotonic microscopy

Imaging of second harmonic generation signals : A tool to explore fibrosis (collagene type I)

Journal of Hepatology 52, 3 (2010) 398-406

Fibrillar collagen scoring by second harmonic microscopy: a new tool in the assessment of liver fibrosis.

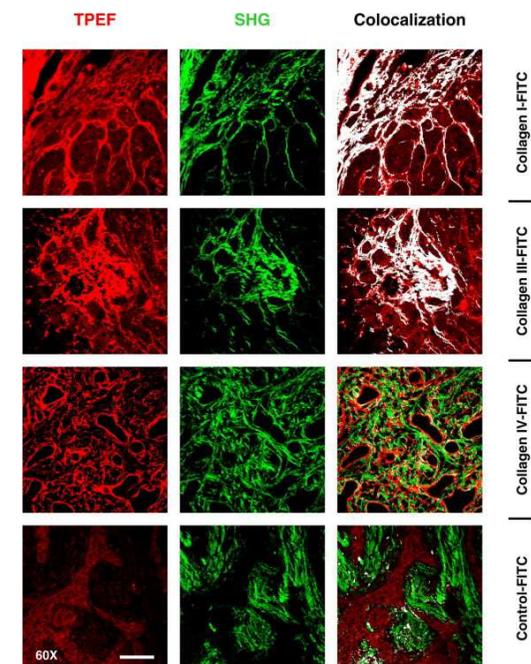
Luc Gailhouste ^{1, 2}, Yann Le Grand ^{3, 4}, Christophe Odin ⁴, Dominique Guyader ^{5, 6}, Bruno Turlin ⁷, Frédéric Ezan ¹, Yoann Désille ⁶, Thomas Guilbert ⁴, Anne Bessard ^{1, 8}, Christophe Frémin ¹, Nathalie Theret ⁹, Georges Baffet ^{1, 9}

We first validated the selectivity of SHG signals for fibrotic deposits (fibrillar collagen type I and III) in human liver by establishing a strong correlation between SHG and immunochemistry assays.

Both frozen fixed or paraffin embedded tissues can be used

SHG scoring gives the opportunity to quantify fibrosis regression in response to an antifibrotic treatment for validating experimental protocols especially for cirrhotic patients

SHG imaging and fibrillar collagen scoring will be applicable to endoscopic systems by using optic fibers coupled with multiphoton microscopy, thus leading to a less invasive procedure for fibrosis evaluation



Biphotonic microscopy



Depth penetration increased
Background signal strongly suppressed
Imaging of living tissue
Molecular interactions by FLIM
Phototoxicity reduced
Second Harmonic Generation



Femtosecond laser very expensive
Difficult to use two pulsed lasers
Resolution 2P 250 nm

Choice of system

	Wide Field Microscopy	Spectral Confocal Microscopy 1P	Confocal Microscopy 2P
Deconvolution	++	+	Not necessary
Simultaneous acquisition of multilabeling	-	++	+/-
Quantitative Imaging	+	+/-	++
Spectral analyses	-	++	++
FLIM	-	+/-	++
Thick Specimen	-	+/-	++
Imaging in vivo	+/-	+/-	++
Second Harmonic Generation	-	-	++

Photonic microscopy with high resolution

Breaking the limit

Abbe limit : $d = \lambda/2$

TIRF : Total Internal Reflexion Microscopy

SIM : Structurated Illumination Microscopy

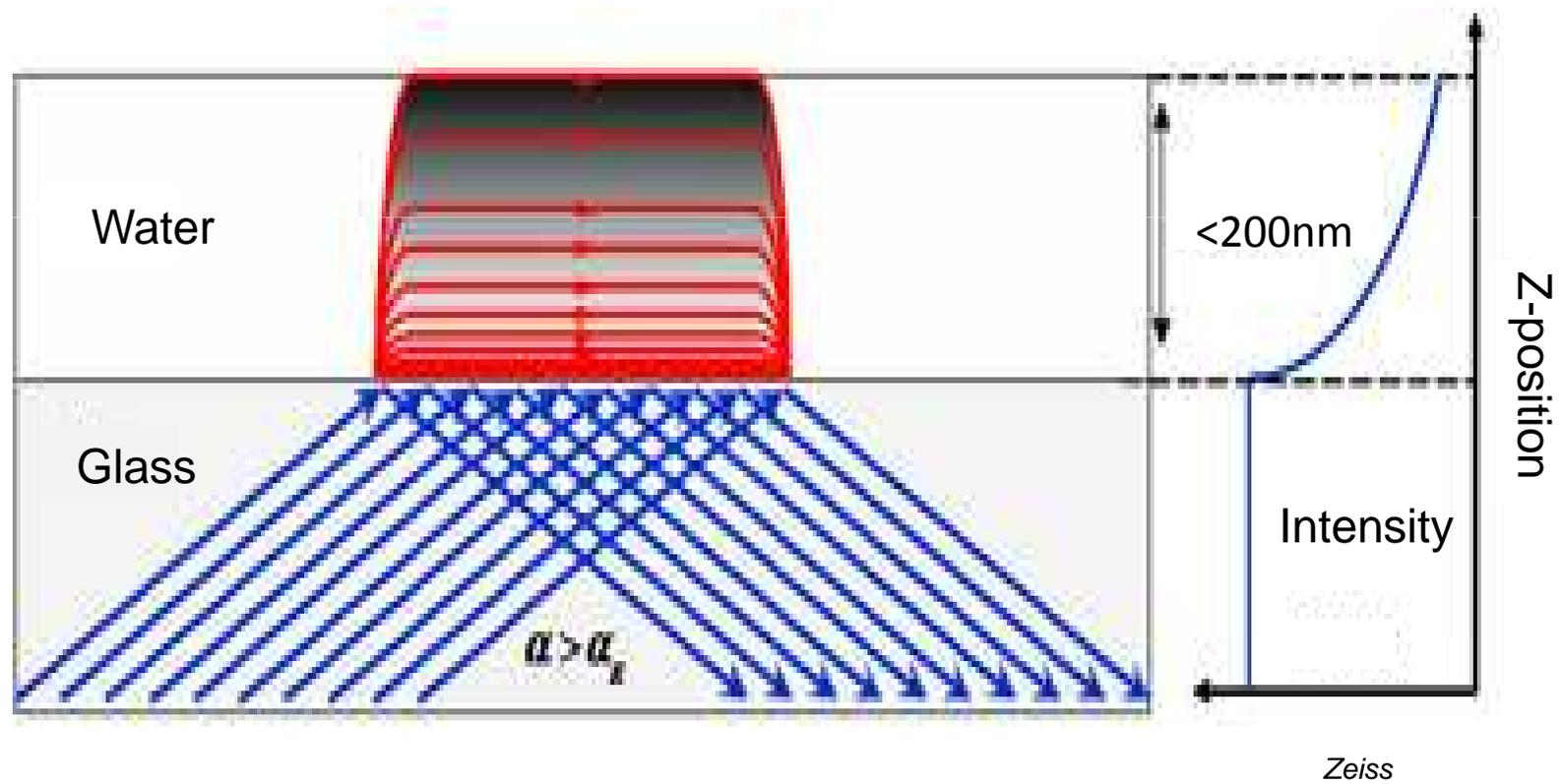
STED : Stimulated Emission of Depletion

PALM : Photoactivation Light Microscopy

TIRF microscopy

TIRF : Total Internal Reflexion Microscopy

Resolution : 80-100 nm



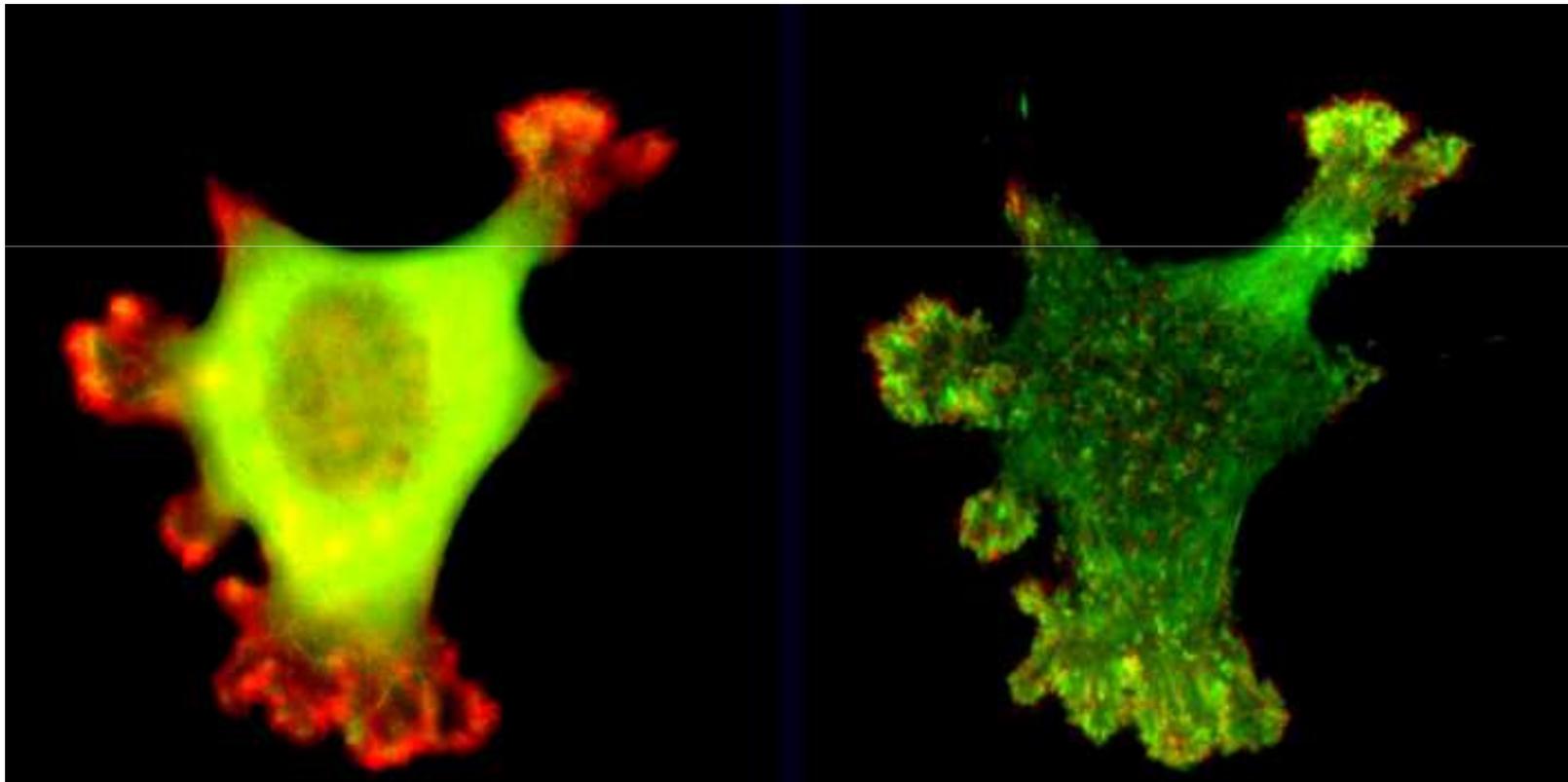
TIRF microscopy

Applications of TIRF microscopy analyses

melanoma cells (mouse)

Confocal microscopy

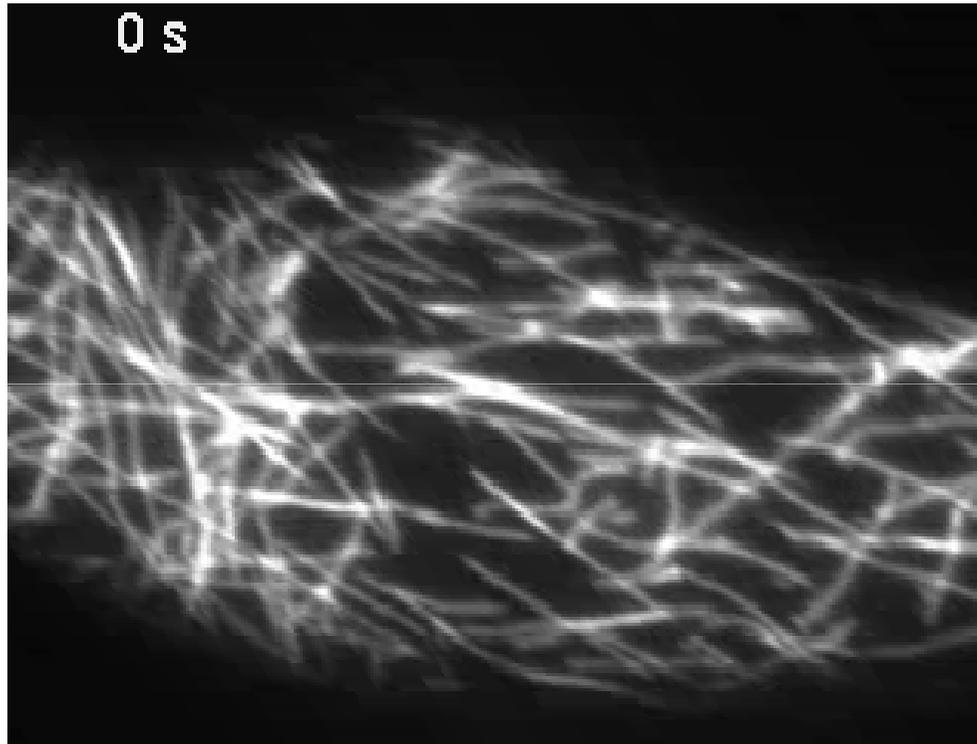
TIRF Microscopy



Myosin green
Actin red

zeiss

TIRF microscopy

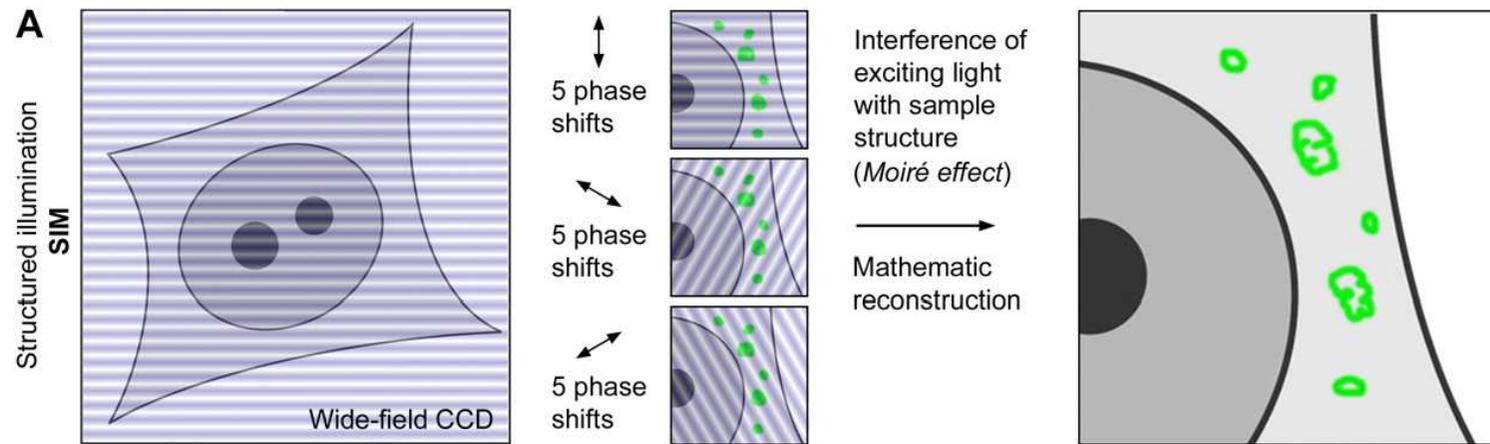


Microtubul eGFP Arabipopsis

SIM : Structured Illumination Microscopy

SIM : Structured Illumination Microscopy

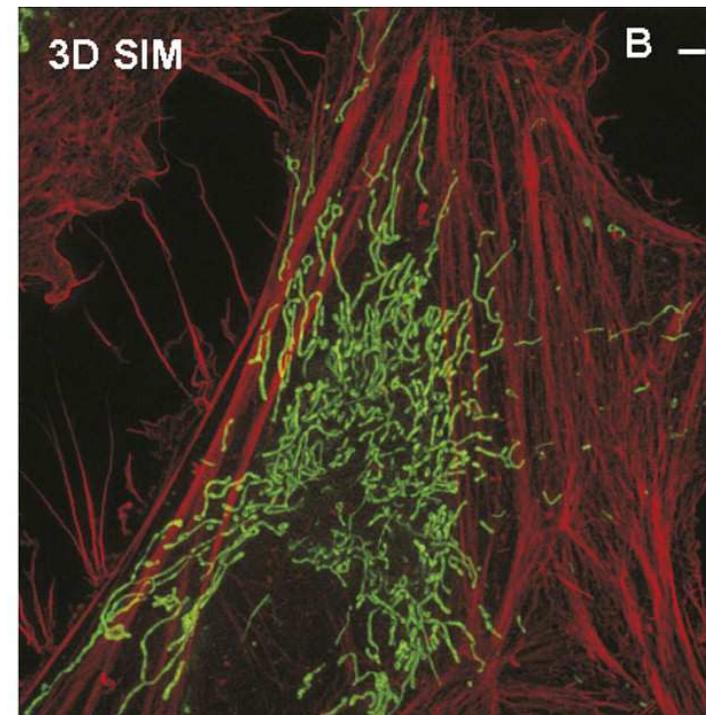
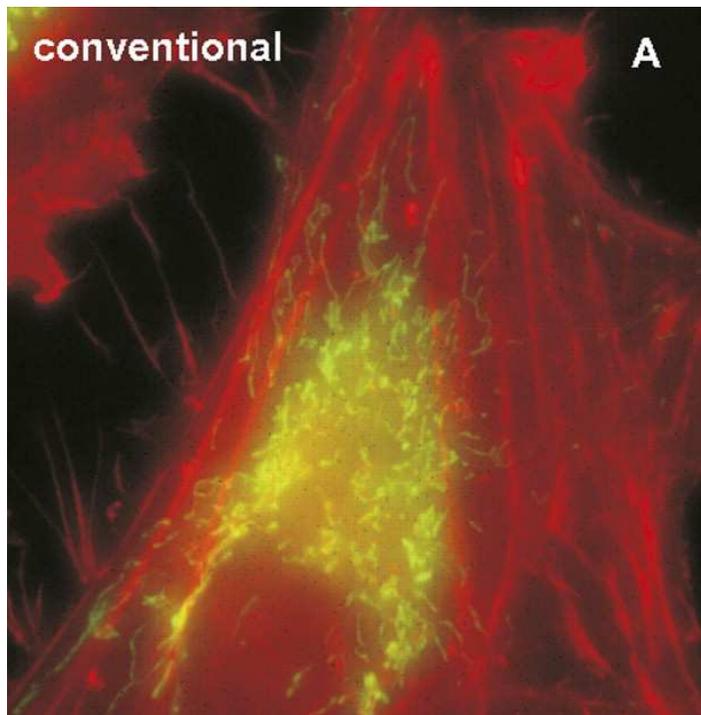
Resolution : 80 - 100 nm



The image detected by the CCD camera thus contains high spatial frequency sample information shifted to a lower spatial frequency band that is transmitted through the objective.

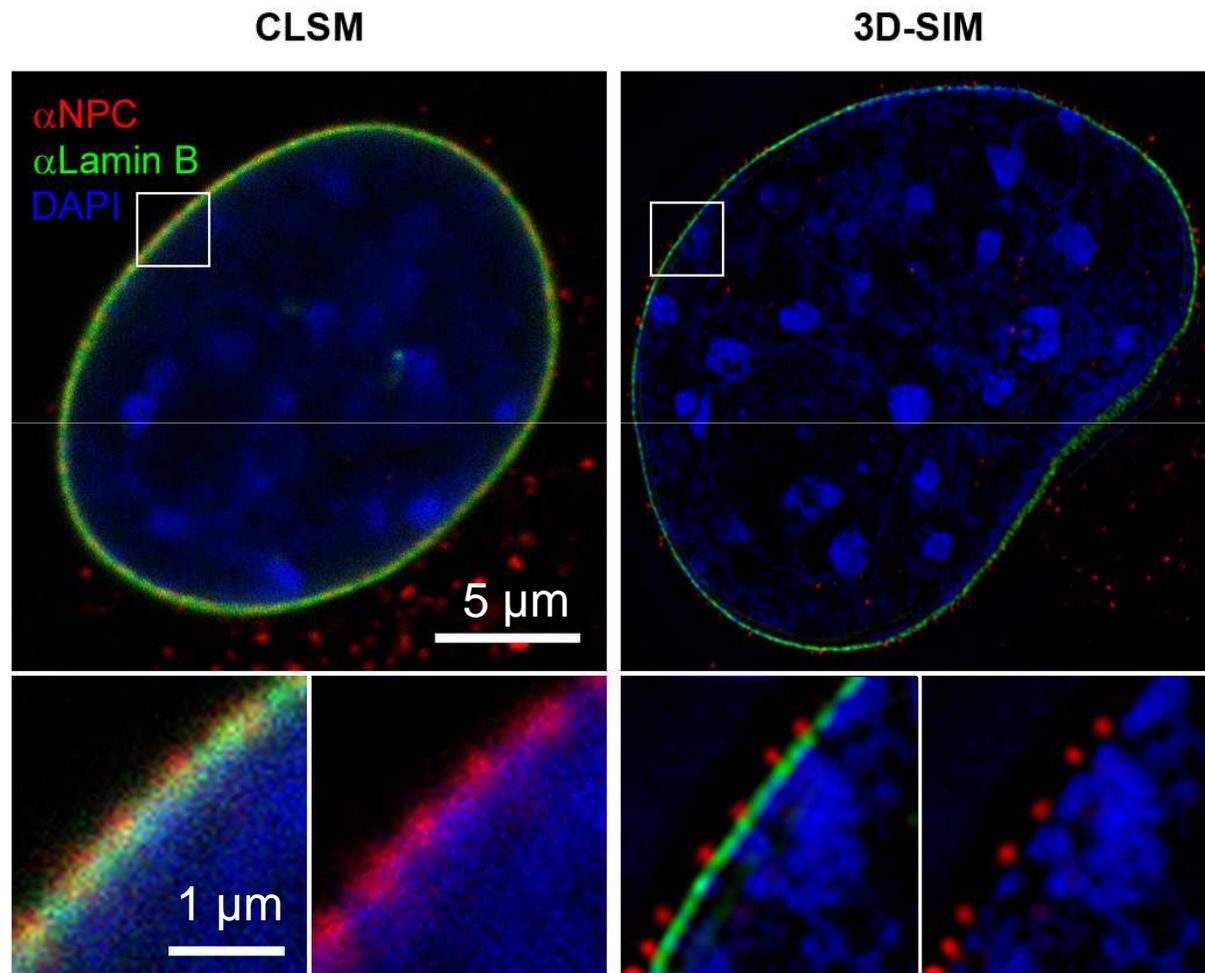
Fluorescence microscopy with high resolution

Applications of SIM analyses



Reto Fiolka and al. PNAS 2012

Fluorescence microscopy with high resolution

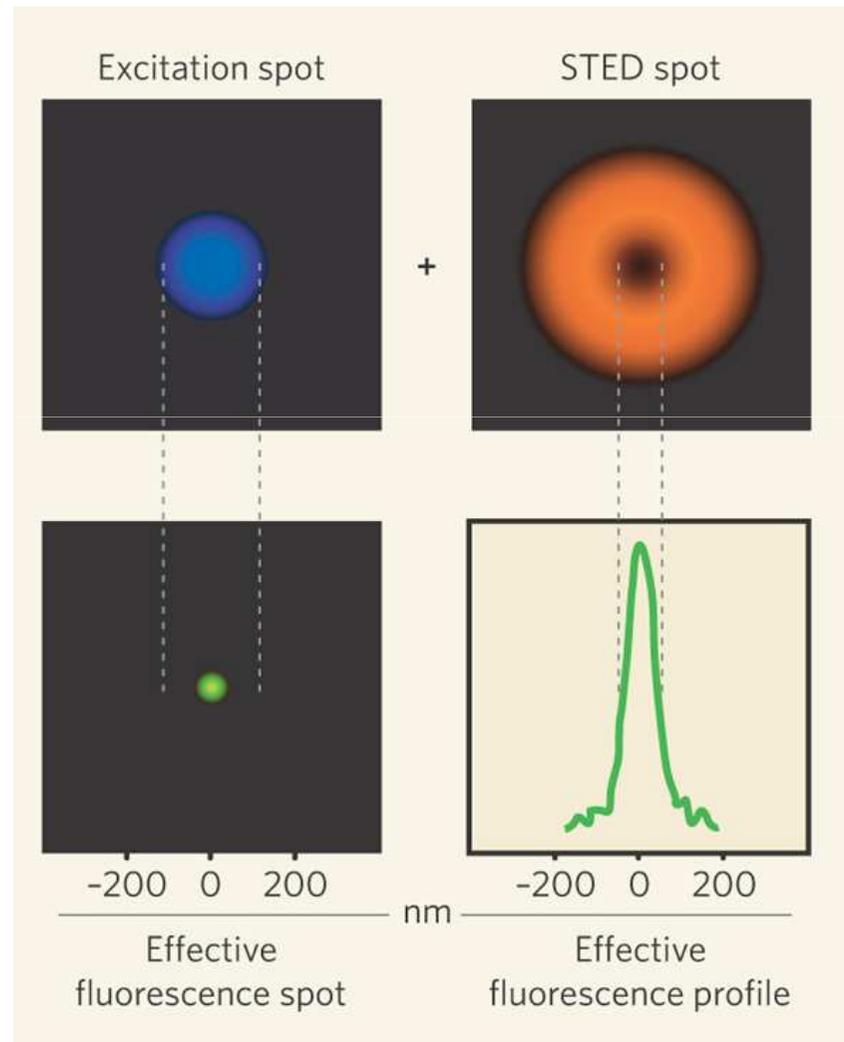


Schermelleh L and al. *Science* 2008

Fluorescence microscopy with high resolution

STED : Stimulated Emission of Depletion

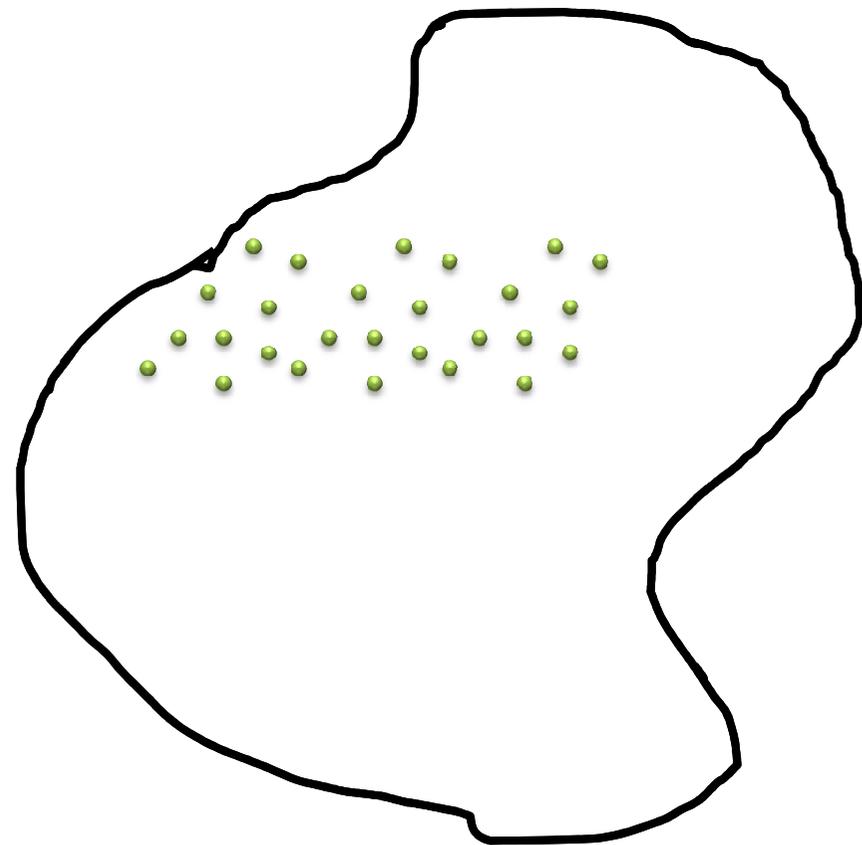
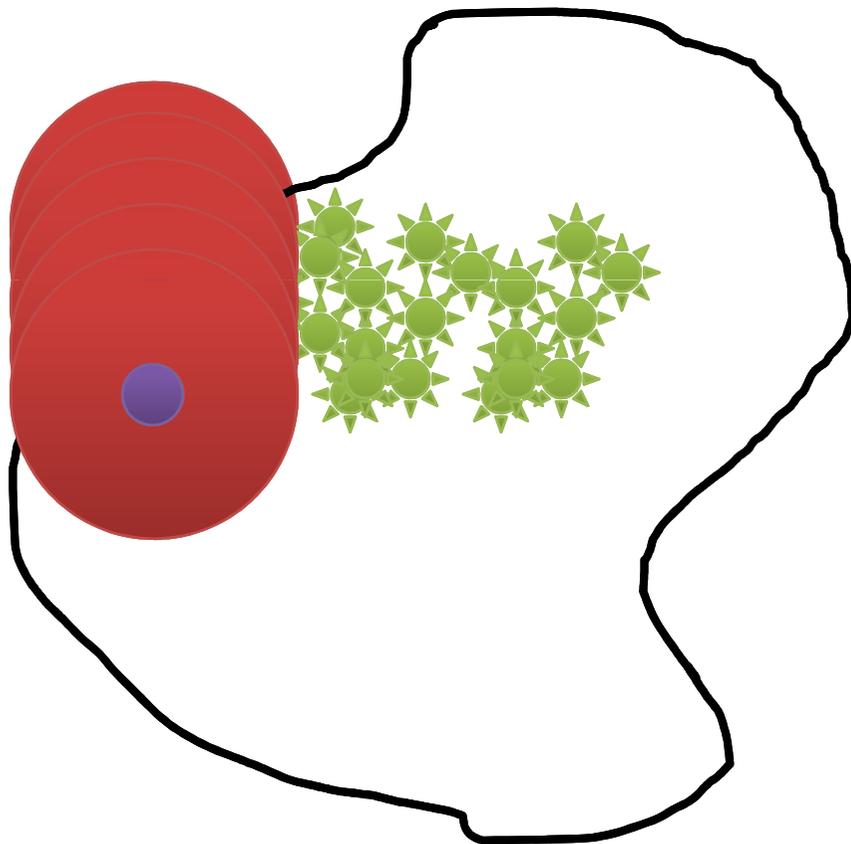
Resolution : 20-40 nm



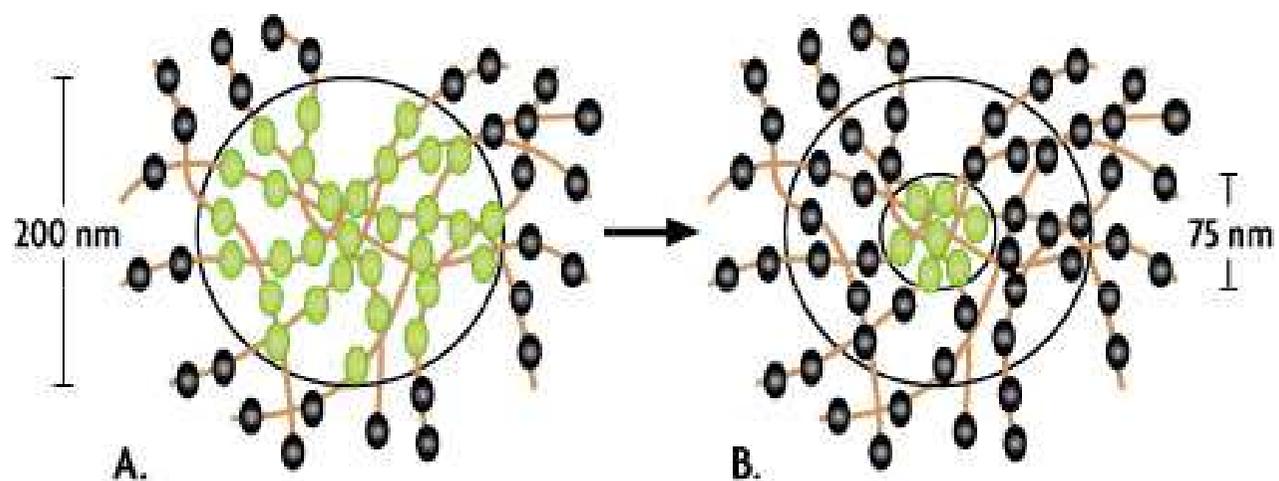
Fluorescence microscopy with high resolution

STED : Stimulated Emission of Depletion

Resolution : 20-40 nm



Fluorescence microscopy with high resolution



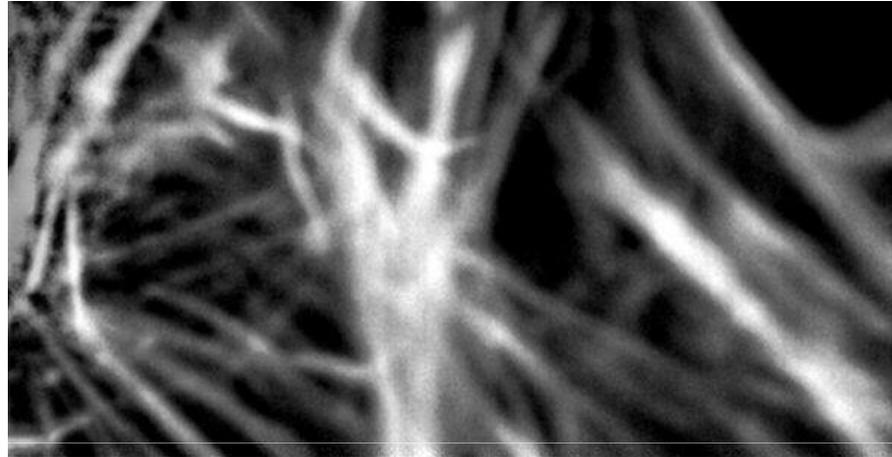
Confocal microscopy

STED microscopy

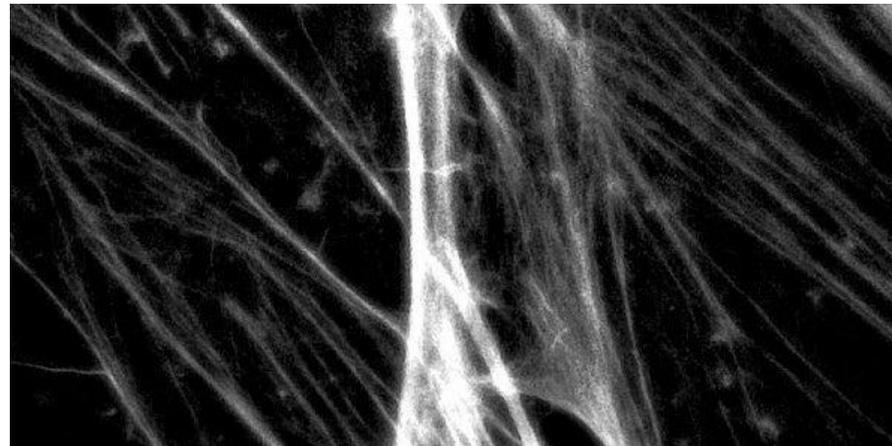
Fluorescence microscopy with high resolution

ACTIN

Confocal microscopy



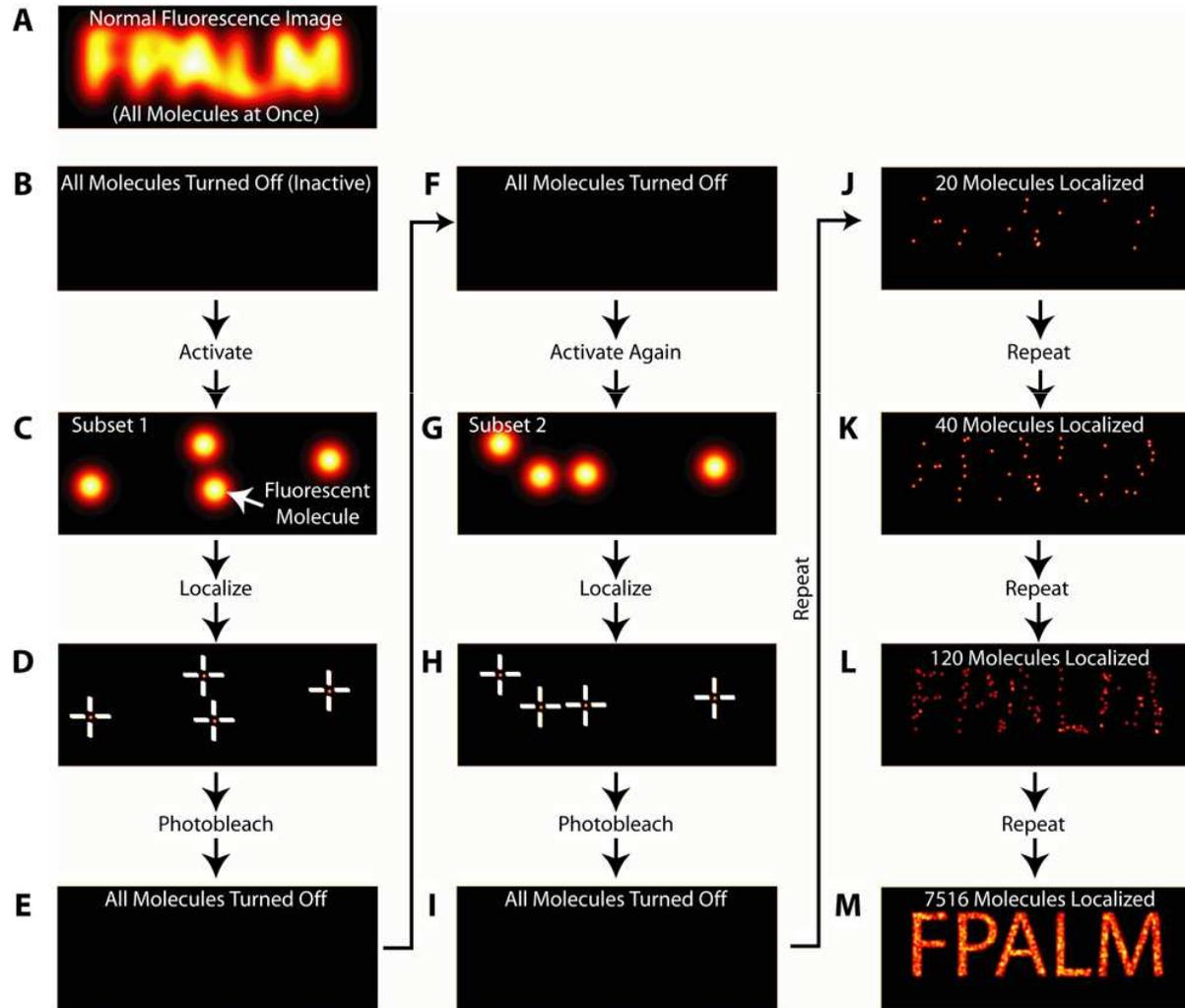
STED microscopy



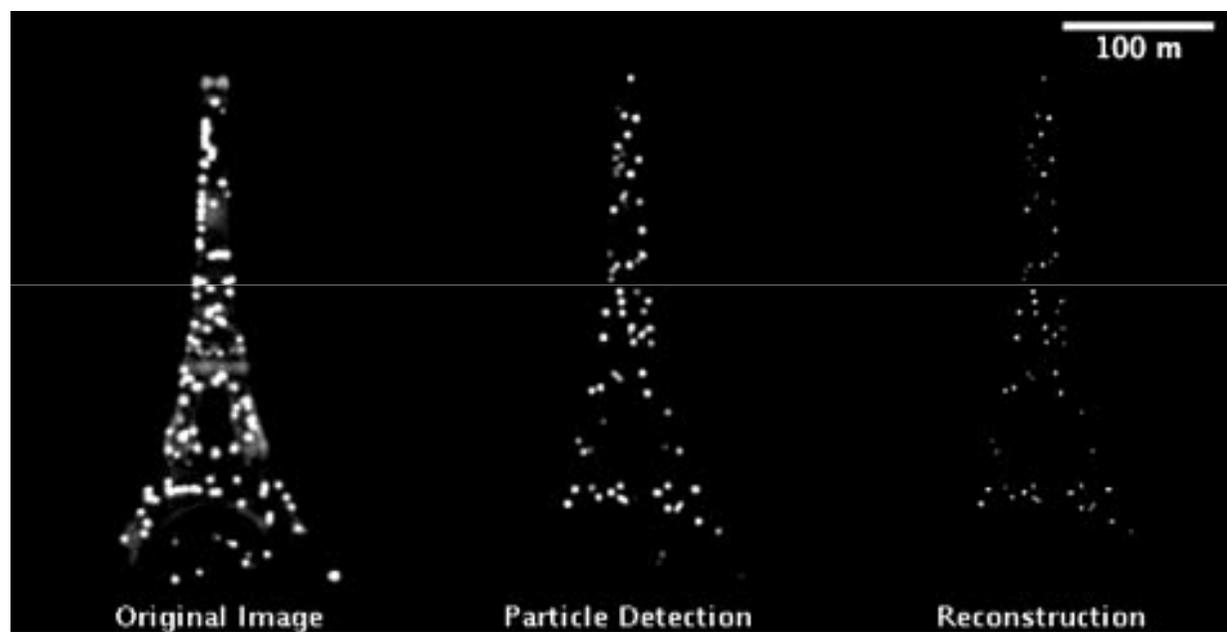
Fluorescence microscopy with high resolution

PALM : Photoactivation Localization Microscopy

Resolution : 20-40 nm

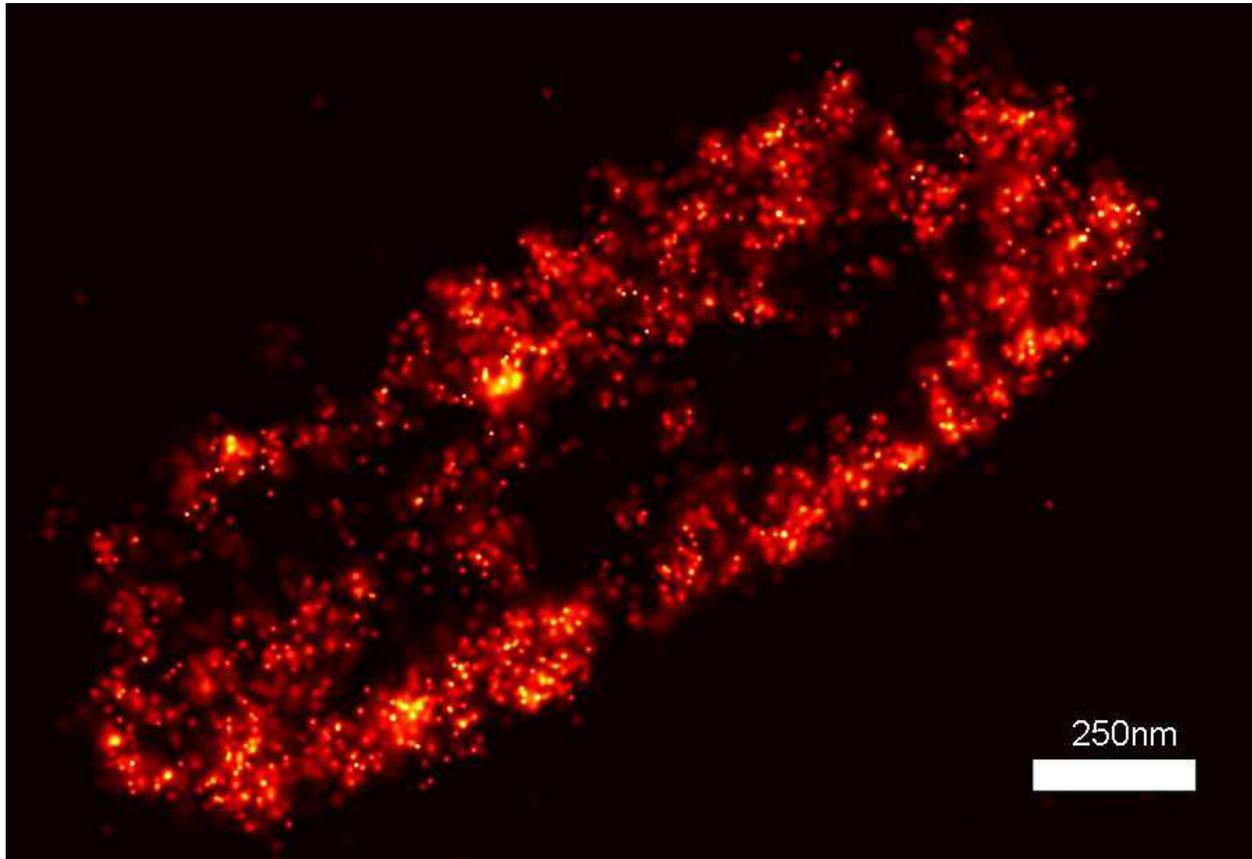


Fluorescence microscopy with high resolution



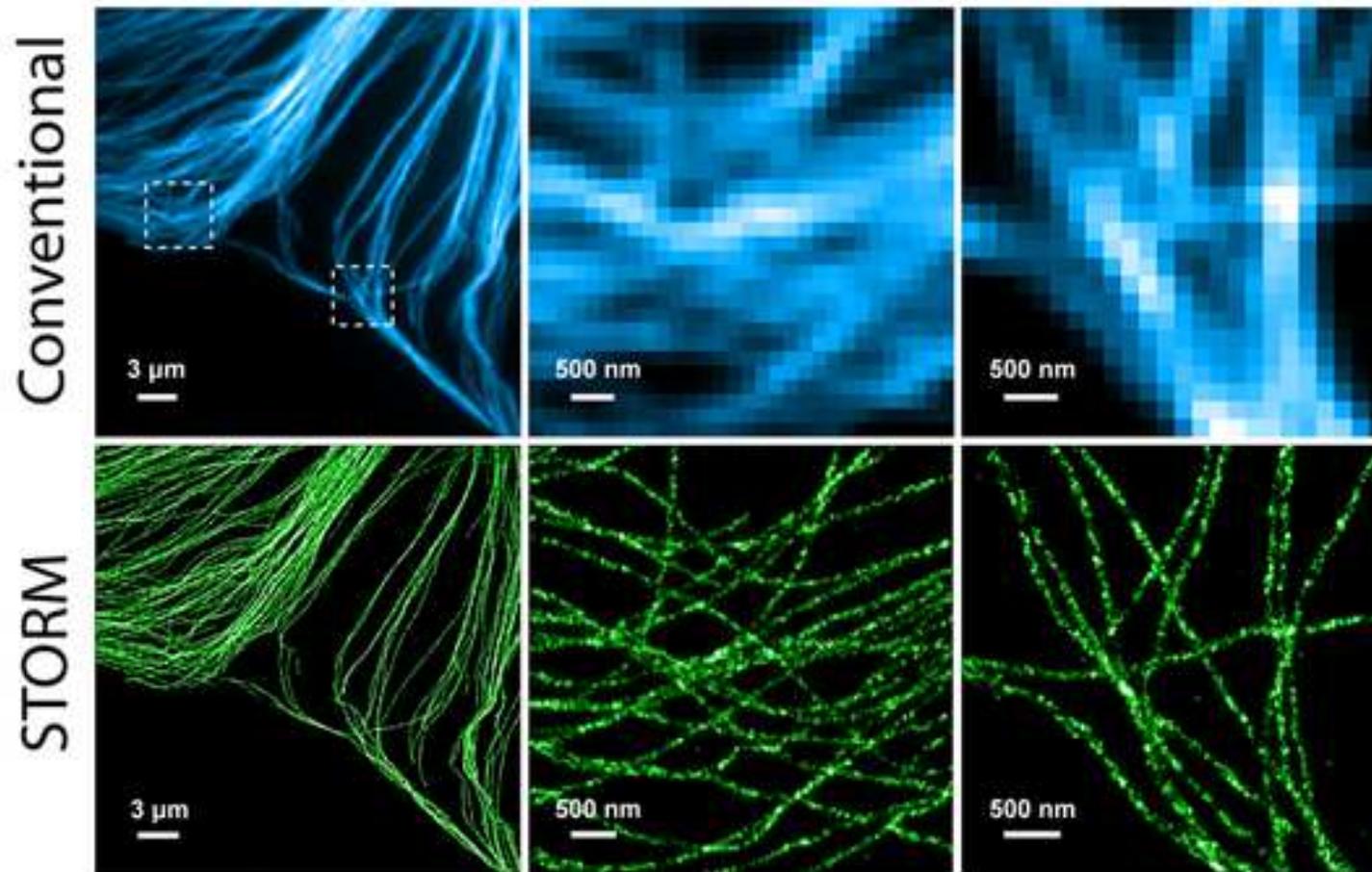
Fluorescence microscopy with high resolution

E Coli Lipo-Poly-Saccharides antibody stained with A647



Stephan Thiberge. Princeton university

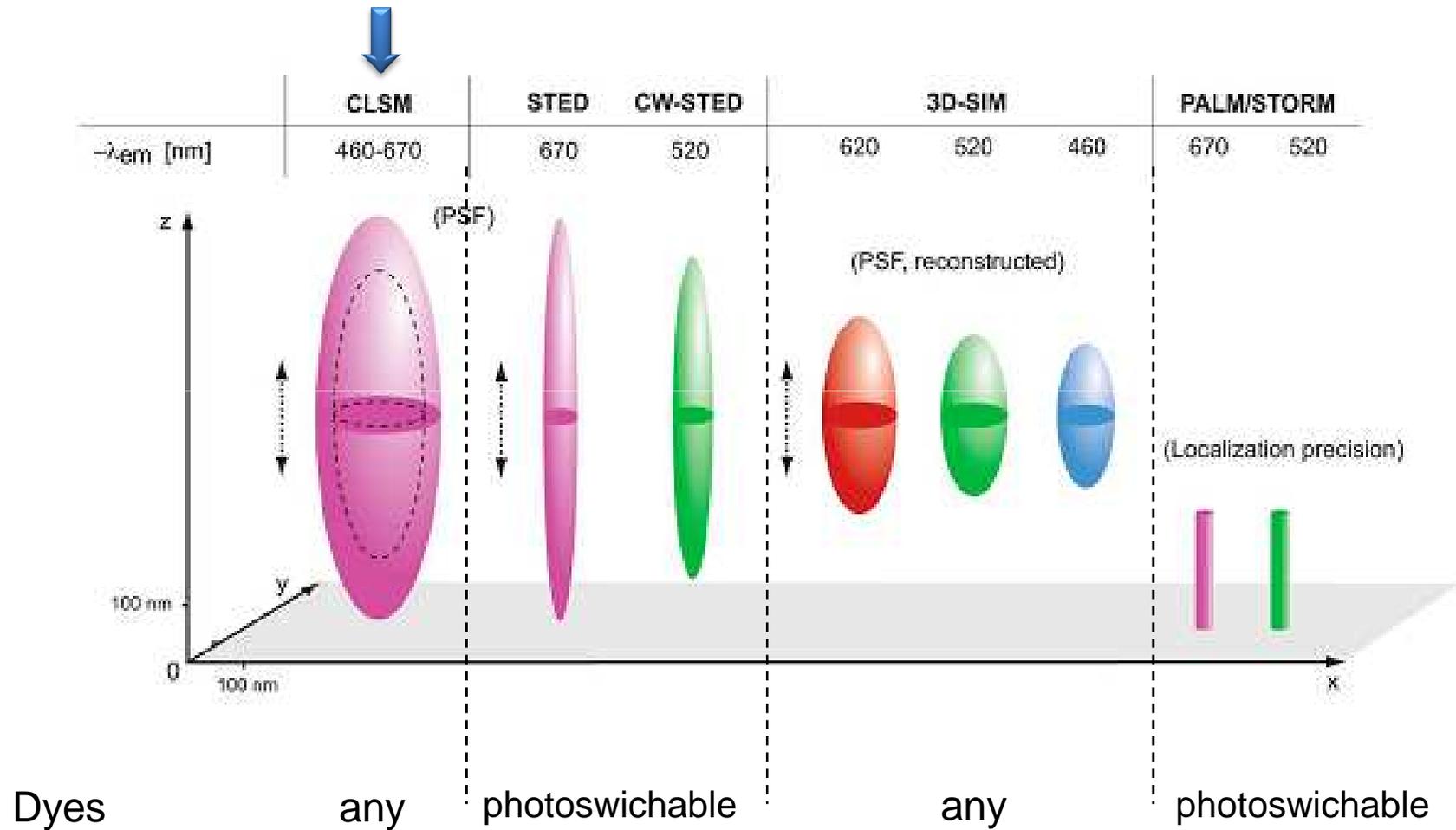
Fluorescence microscopy with high resolution



Science (2007)

Fluorescence microscopy with high resolution

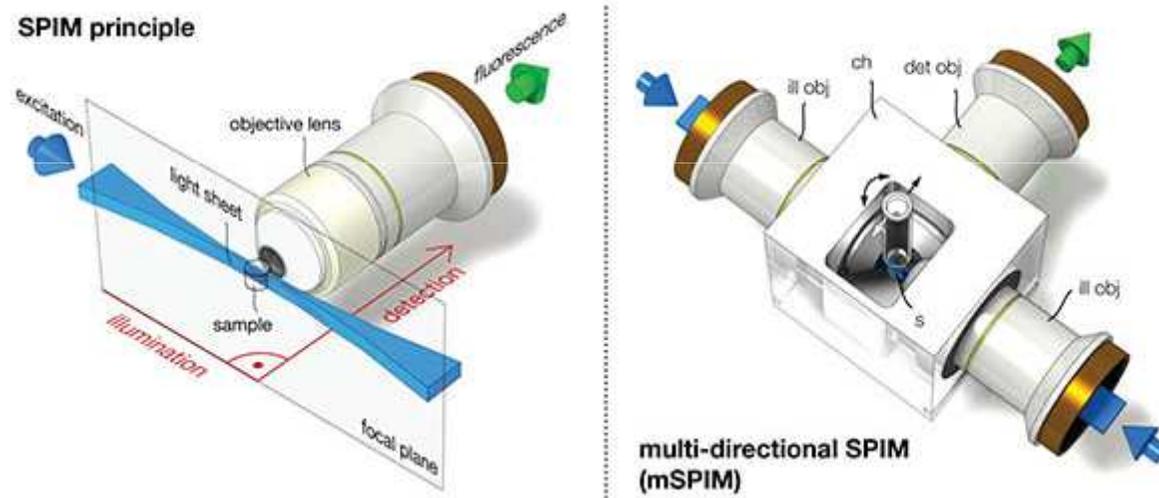
Breaking the limit



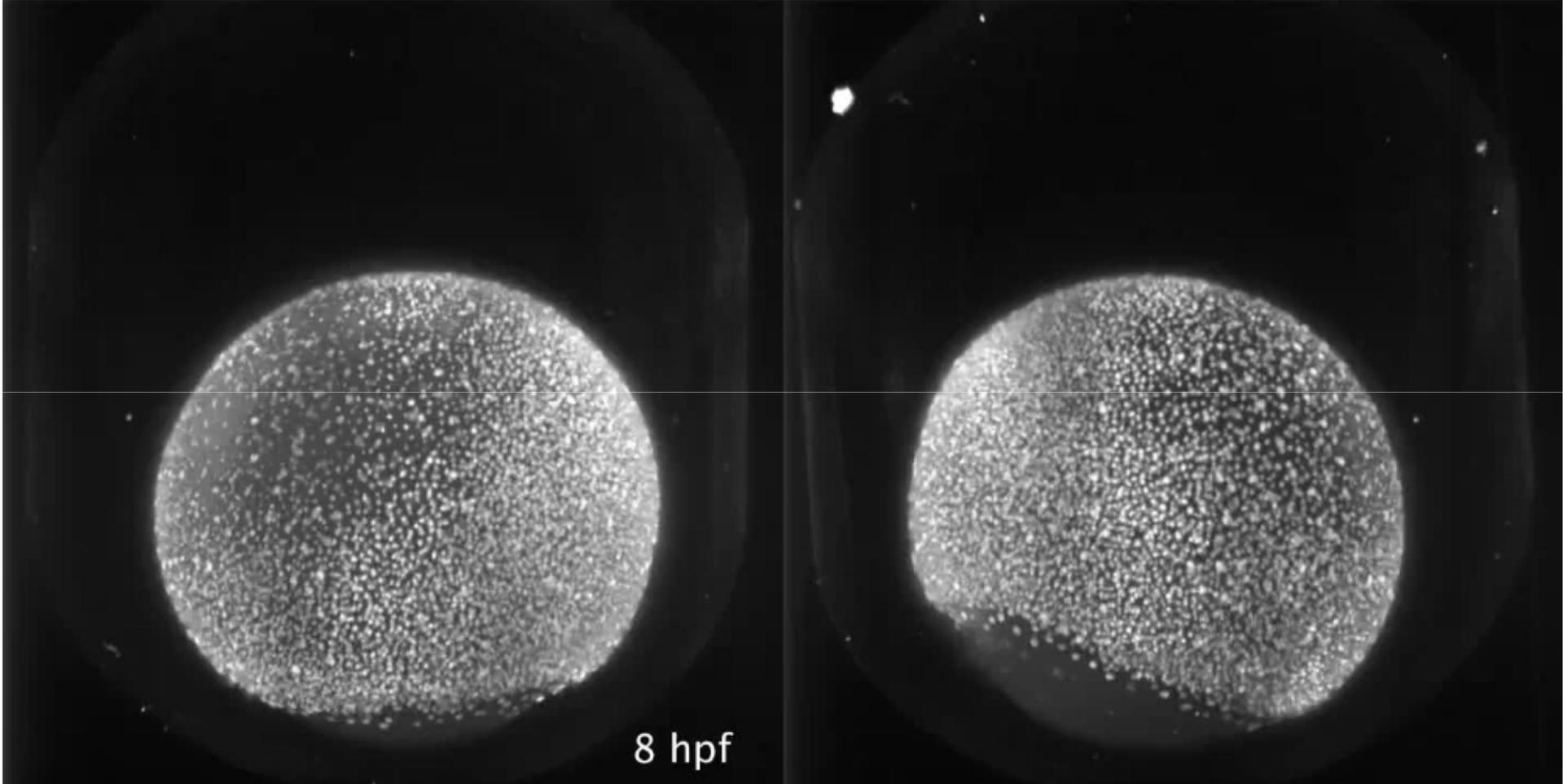
Choice of system

	Confocal	TIRF	SIM	STED	PALM
X-Y resolution	200	80-100	80-100	20-40	20-40
Z resolution	400-500	200	200	400-500	20-40
Dyes	Any	Any	Any	Photo switchable	Photo switchable
Rapidity	+	+++	-	++	-
Simultaneous colors	>3	3	>3	2	2
Post processing	No	No	Yes	Yes	Yes

Selective plane illumination microscope



the Huisken Lab, Max Plank Institute

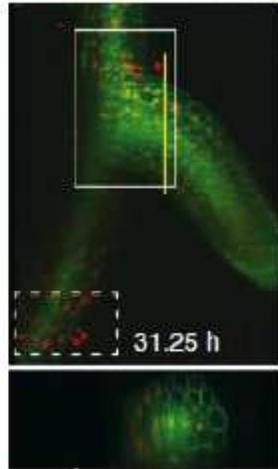


Molecular & cellular biology



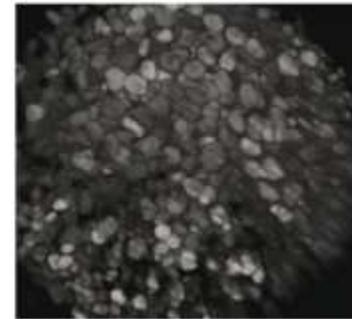
Capoulade & *al.*, 2011

Plant biology



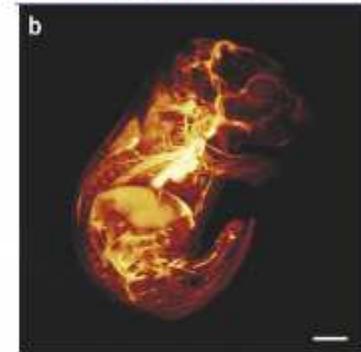
Maizel & *al.*, 2011

Cancer biology



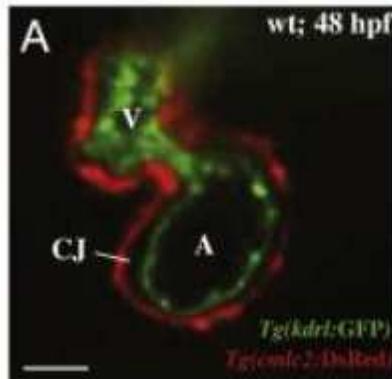
Lorenzo & *al.*, 2011

Neuroscience

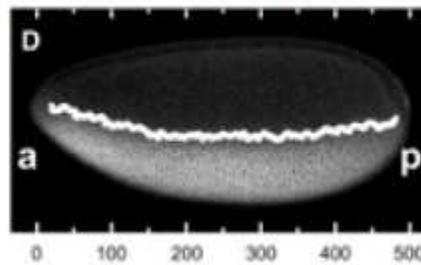


Dodt & *al.*, 2007

Developmental biology

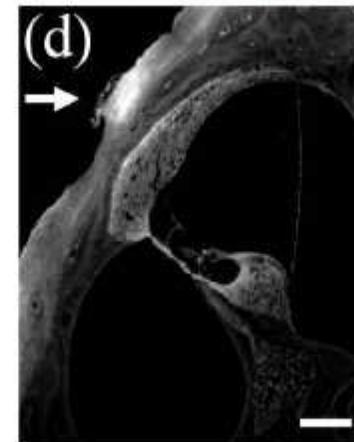


Mellman & *al.*, 2012



Reeves & *al.*, 2012

Anatomical studies



Schröter & *al.*, 2012